

# GATE Applications

## Respiratory Motion in PET

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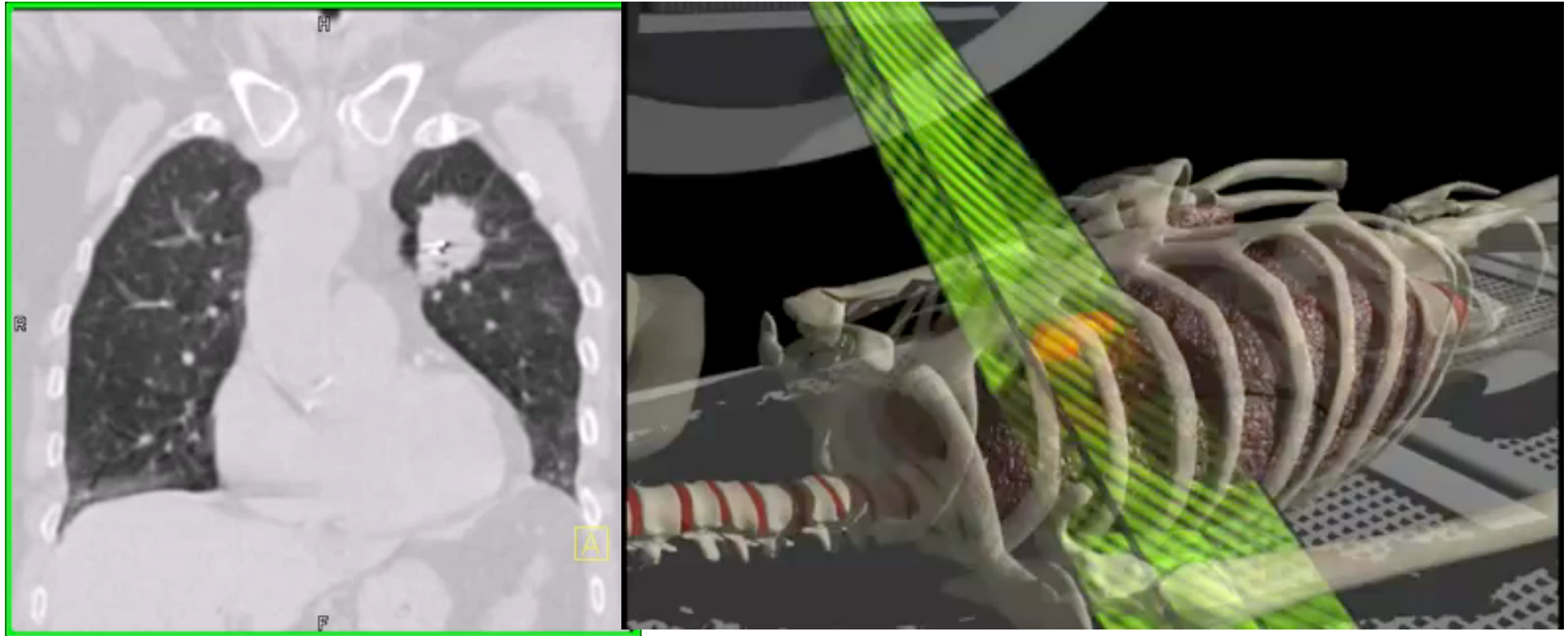
8th December, 2008

ANZSNM Physics SIG, ACPSEM Nuclear Medicine Physics SG Meeting MonteCarlo Applications in  
Nuclear Medicine and Radiotherapy



**Austin Health**

# Respiratory Motion

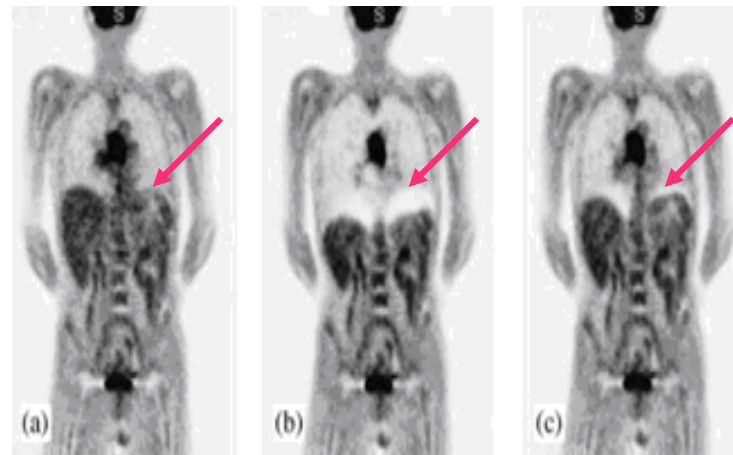
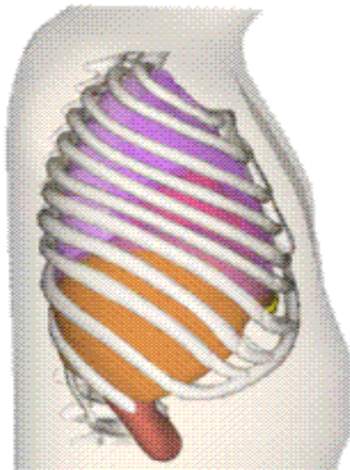


- Respiratory motion in PET
  - In lung, up to 20 mm

# Respiratory Motion

## Attenuation Correction Artifact

- Respiratory motion issue
  - Free breathing cycles during PET acquisition data cause blurring images
  - Attenuation correction artifact



*Nuclear Instruments & Methods in Physics Research A 569 2006, 453-457*

# Respiratory Motion

## Lesion Localisation

- Effect of Respiratory Motion on Tumour



Average over all respiratory phase.

Exhalation phase.

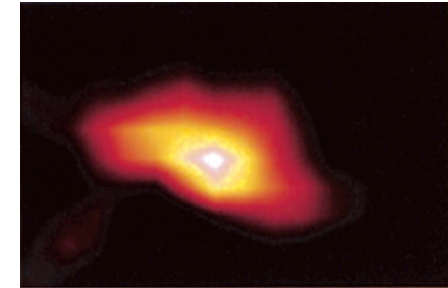
[www.fzd.de](http://www.fzd.de) : Forschungszentrum Dresden / Rossendorf

# Respiratory Motion

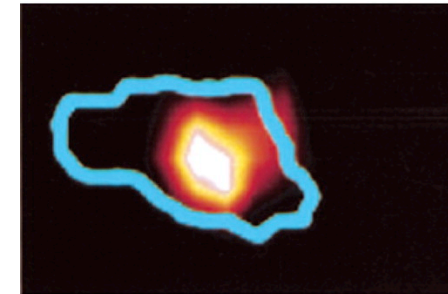
## Tumour Volume Estimation

- Transaxial  $^{18}\text{F}$ -FDG PET Image
  - a) Non-gated Mode
  - b) Gated mode
  - c) Planning target volume in non-gated (light blue) and gated (pink)

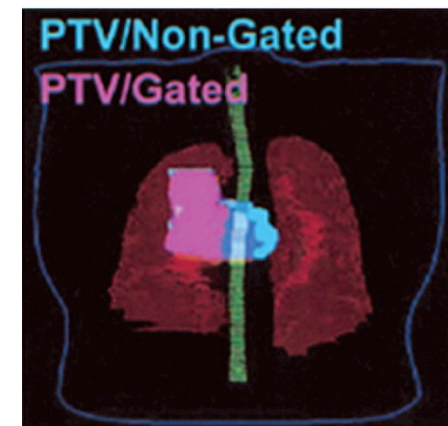
Nehmeh S, Erdi Y, Ling CC, et al.  
Effect of respiratory gating on quantifying PET images of lung cancer.  
J Nucl Med 2002;43:876–81



(a)



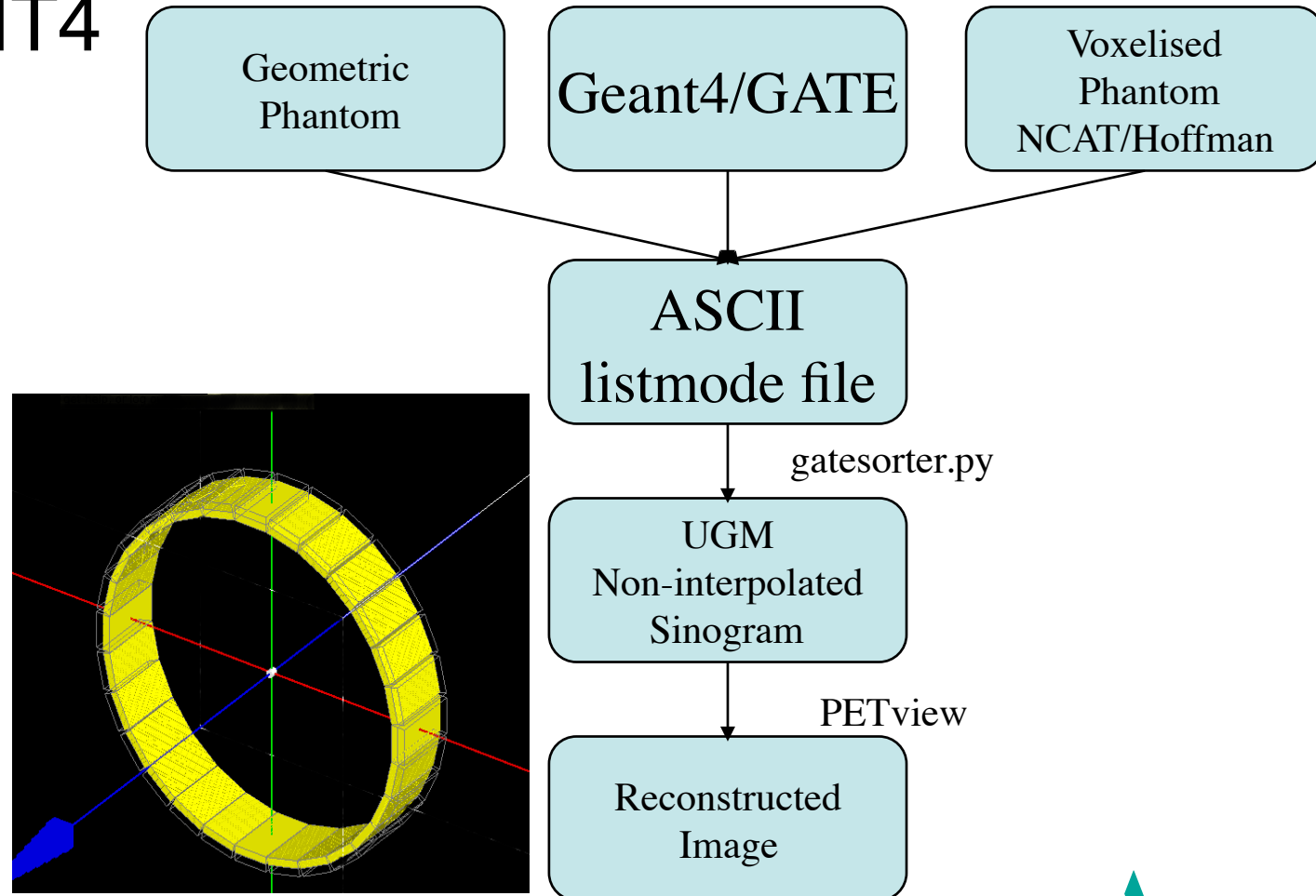
(b)

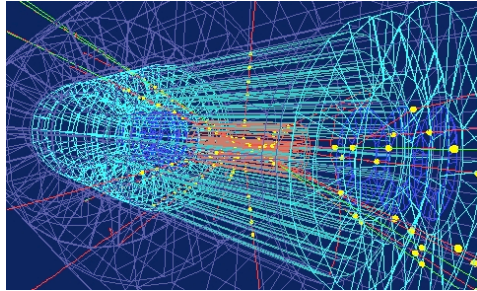


(c)

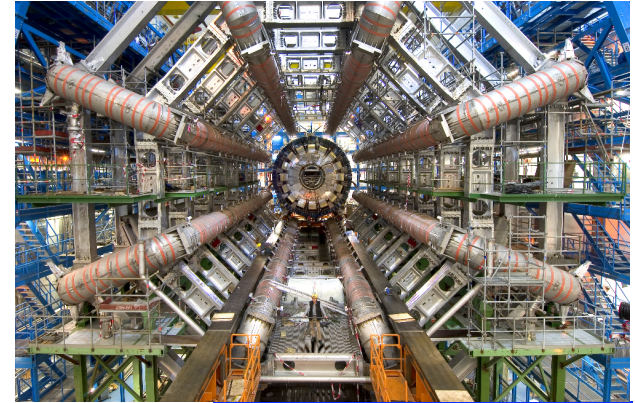
# Method and Materials

- GEANT4
- GATE

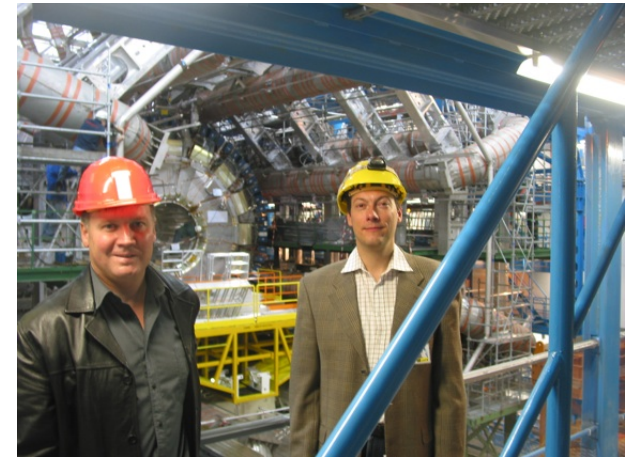
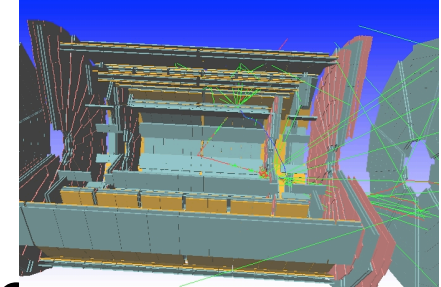




# Geant4/GATE



- **GEANT**
  - **GE**ometry **ANd** **T**racking
  - 1974 Project Initiation
  - 3.21 / 2000 – last FORTRAN release
- **Geant4**
  - 1994 Project Initiation
    - C++ – Object Oriented Design
  - 1998 – 0.0 release
  - 2008 – 9.1 release



# Geant4

## ATLAS Detector



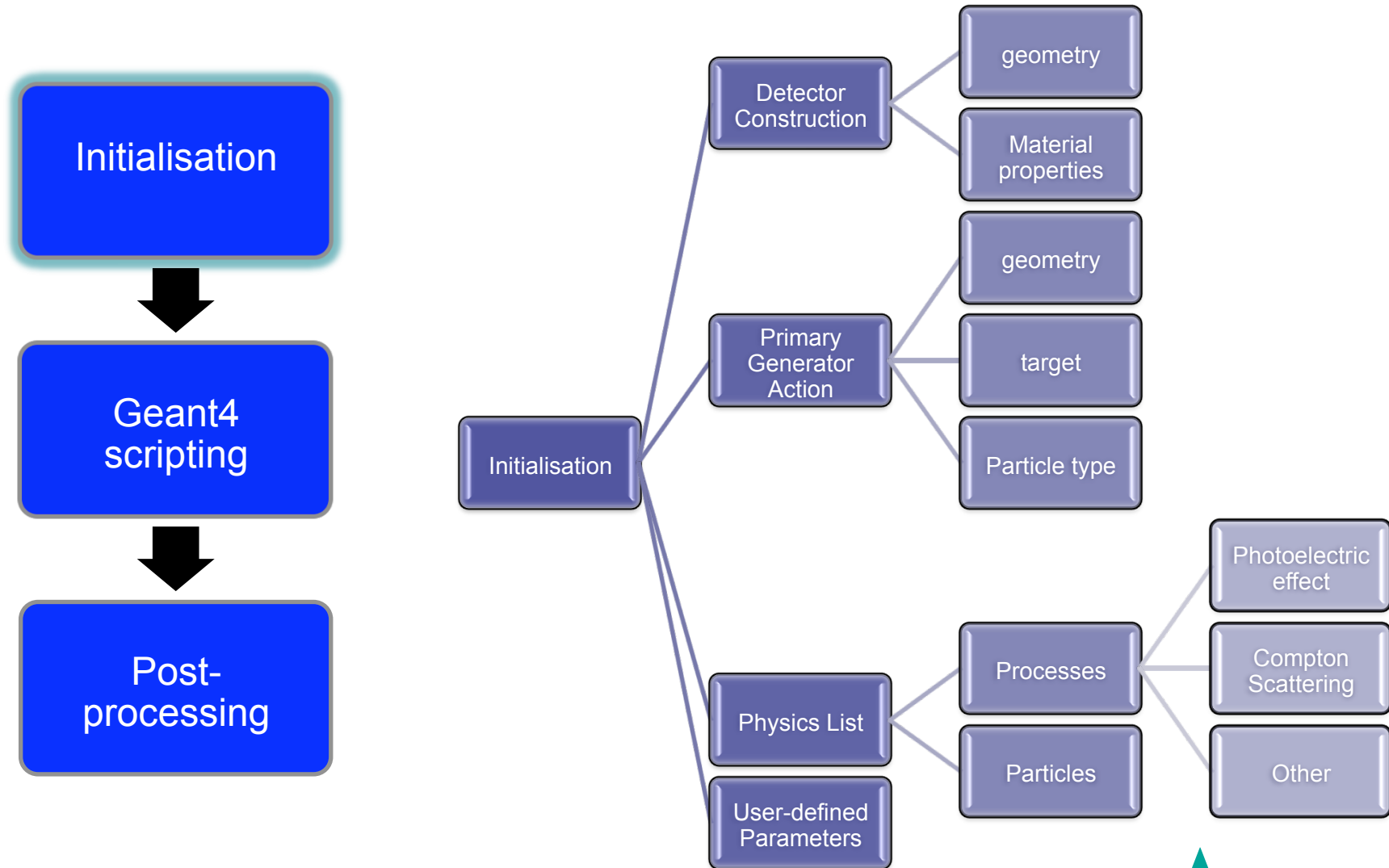
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**Austin Health**

# Geant4 object model



# GATE

## Geant4 Application Tomographie Emission

- 2001 – Project Initiation  
– Irene Buvat
- 2002 – 1.0.0
- 2004 – 1.0.1
- 2005 – 1.1.0-**2.2.0** / 6.2.p02 – **6.9.p02**
- 2006 – 3.0.0 / 8.1.p02
- 2008 – 4.0.0 / 9.1.p03



# GATE

## Installation

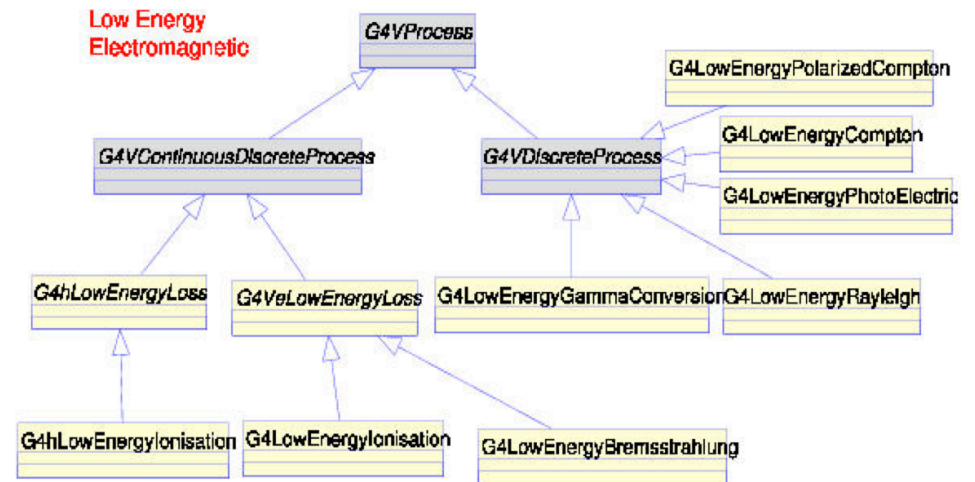
- Platforms
  - Linux, OS X, Unices, Windows/CygWin
- Requirements / Dependencies
  - gcc 4.x
  - Xwindows
  - CLHEP
  - Geant4 + G4EMLOW data
  - ROOT
  - LMF
  - ECAT
  - ***Lots of Patience!***

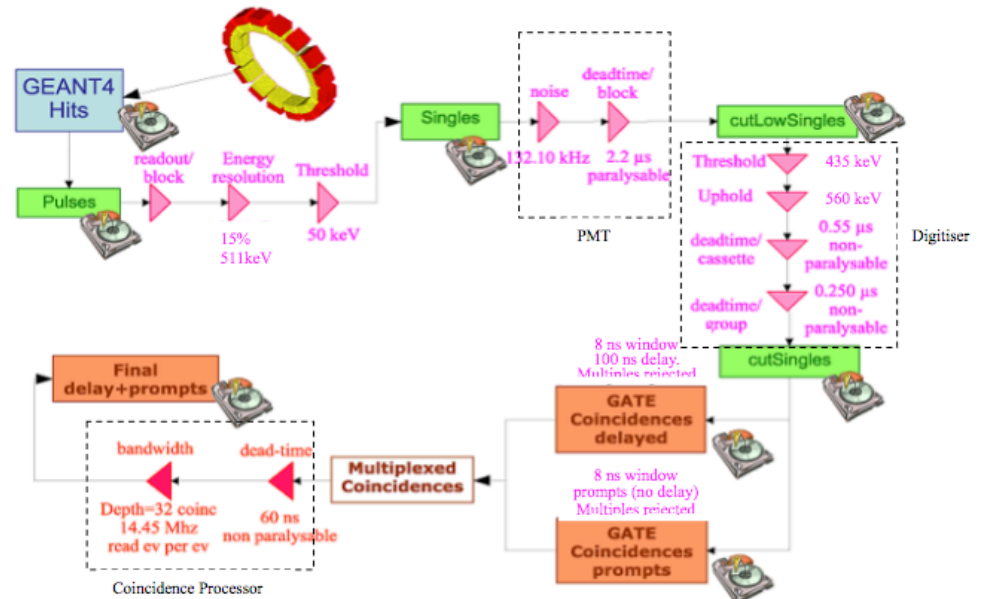
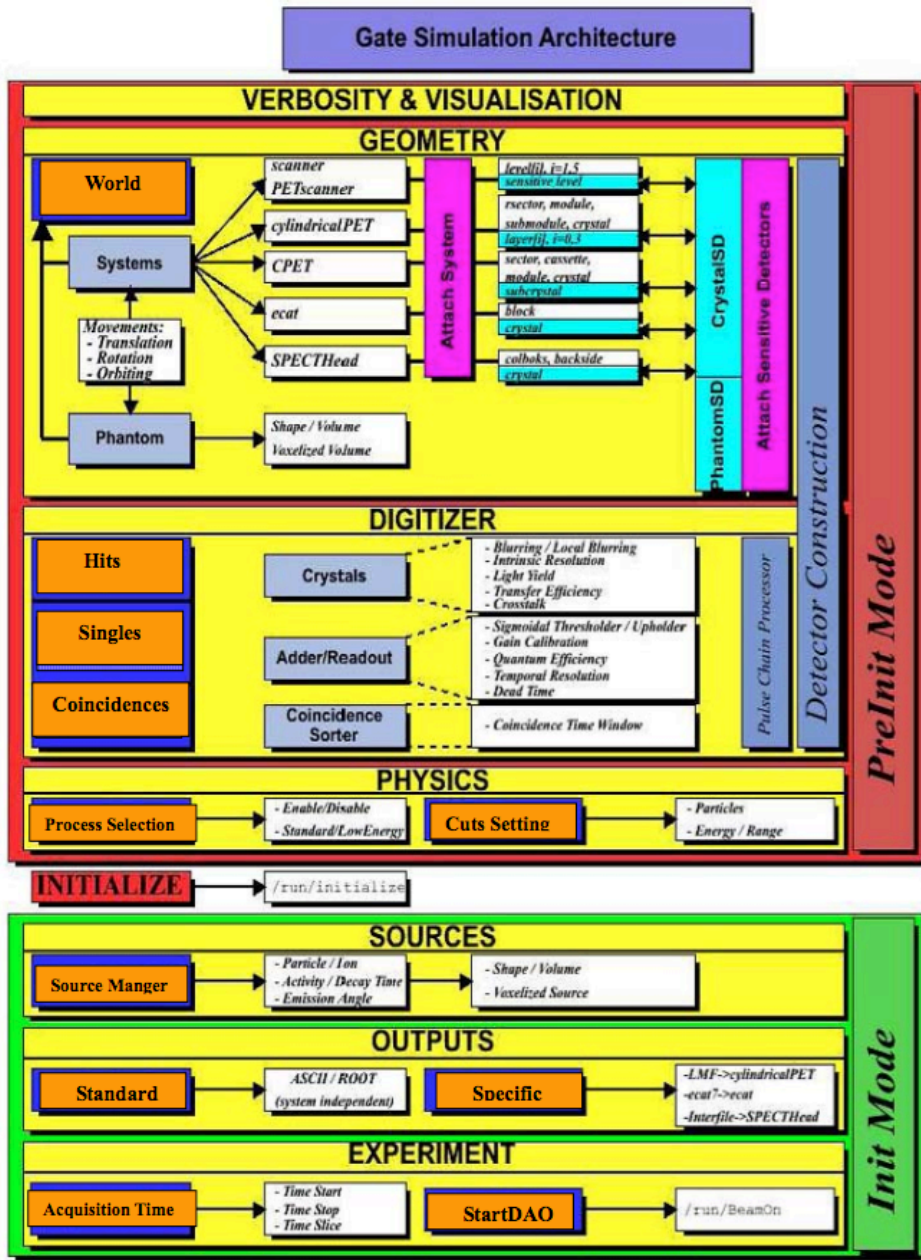


# Geant4

## Data Files

- G4ABLA.3.0
  - Nuclear Shell Effects
- G4EMLOW.5.1
  - Low Energy Electromagnetic Processes (250 eV to 10 GeV)
    - Rayleigh Scattering
    - Compton Scattering
    - Photo-electric
    - Pair-production
- Neutron Processes
  - G4NDL.0.2
    - without thermal neutron reaction channels
  - G4NDL.3.12
    - with thermal neutron reaction channels
- G4RadioactiveDecay.3.2
  - Hadronic radioactive decay processes
- PhotonEvaporation.2.0
  - Photon Evaporation Reaction Channels





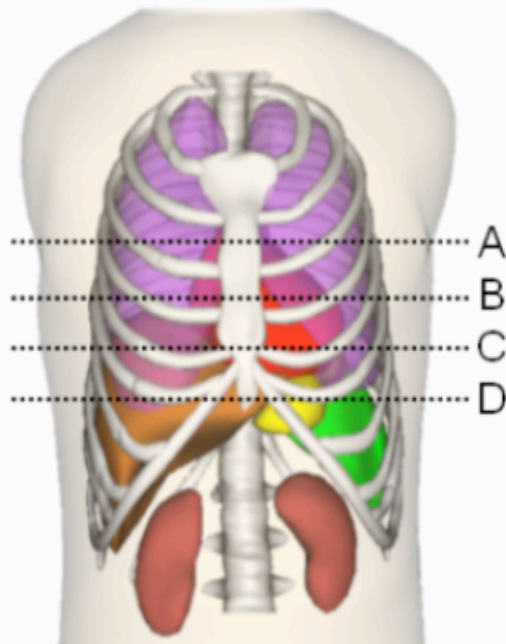
# Respiratory Motion

- Scanner specification
  - Allegro / Gemini
- Validation
  - Physical Phantoms
- Phantom specification
  - Geometric (gate) objects
  - Voxelised 4D-NCAT



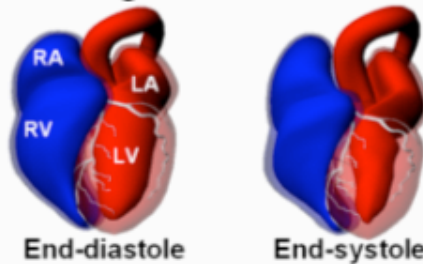
# 4D NCAT

## 4D NCAT

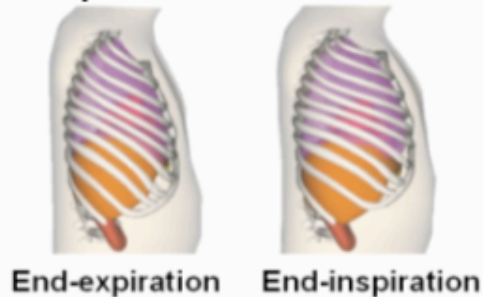


## Motion Models

### Beating Heart

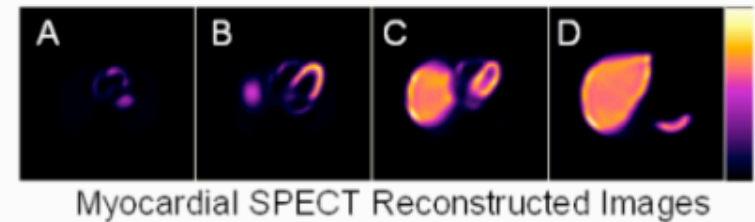


### Respiration

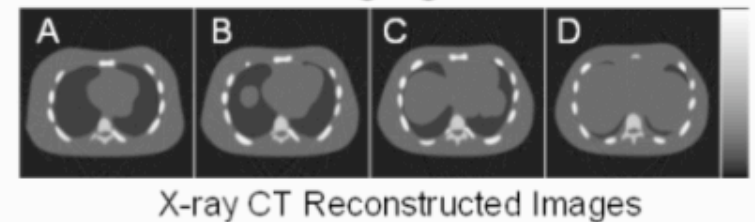


## Simulations

### Emission Imaging



### Transmission Imaging



- [http://dmip.rad.jhmi.edu/people/faculty/Paul/Segars\\_research.htm](http://dmip.rad.jhmi.edu/people/faculty/Paul/Segars_research.htm)

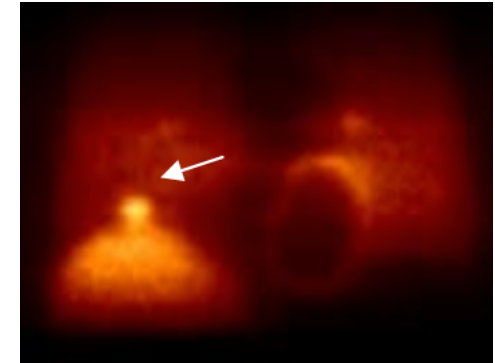
# 4D NCAT

- Developed by Segars
  - 3D surfaces of torso structures
    - MRI & hi-res respiratory-gated CT
  - Heart motion
    - 4D cubic NURBS
      - Non Uniform Rational B-Splines
  - Respiratory Motion
    - Modelled on Normal Tidal Breathing
  - Compressible motions
    - Lung, Liver, Heart

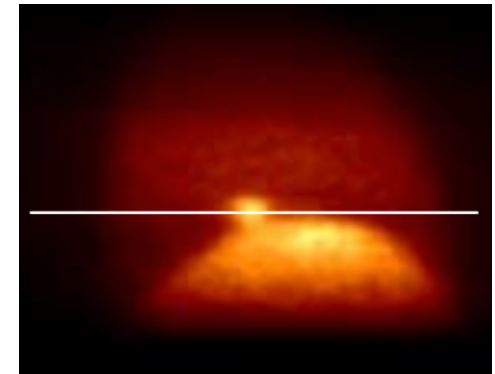


# 4D NCAT

- Lesion models
  - resp\_lesn\_bin : lesion generator
- Dynamic output
  - User defined times
  - Output as binary
    - Converted to Interfile for GATE



Coronal view: heart/lung/liver/lesion

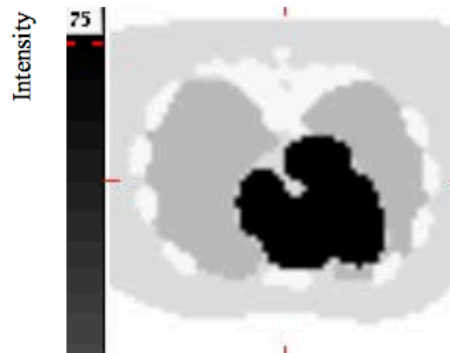


Sagittal view: liver/lung/lesion

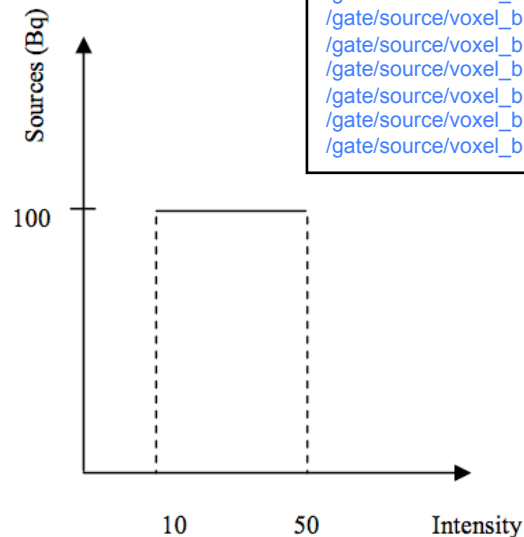
# GATE

## Voxelised Phantoms

- Translation tables
  - Source
  - Attenuation



(a). Intensity value = 10 ~ 50 in the voxelised phantom



(b). Intensity value = 10 ~ 50 converted to source activity = 100 Bq

```
# VOXEL SOURCE BASED ON THE NCAT PHANTOM
/gate/source/addSource voxel_brain voxel
##### Range translator
/gate/source/voxel_brain/reader/insert interfile

##### Linear translator: All numbers directly #into activities
/gate/source/voxel_brain/interfileReader/translator/insert linear
/gate/source/voxel_brain/interfileReader/linearTranslator/setScale 10.50 Bq

/gate/source/voxel_brain/interfileReader/readFile lung_lesn.h33

/gate/source/voxel_brain/setType backtoback
/gate/source/voxel_brain/gps/particle gamma
/gate/source/voxel_brain/setForcedUnstableFlag true
/gate/source/voxel_brain/setForcedHalfLife 6586.2 s
/gate/source/voxel_brain/gps/energytype Mono
/gate/source/voxel_brain/gps/monoenergy 0.511 MeV
/gate/source/voxel_brain/setPosition -160. -160. -160.mm # 64*64*64;0.5mm
/gate/source/voxel_brain/gps/confine NULL
/gate/source/voxel_brain/gps/angtype iso
/gate/source/voxel_brain/dump 1
```

# GATE Configuration

## Scanner Descriptor Macro

- Physics
  - Photo-electric + Compton
- Detectors
  - Geometry
  - Materials
- Sources
  - Geometry
  - Energy



# GATE Configuration

## Jazczack Source Descriptor Macro

```
/gate/source/addSource F18PointA  
/gate/source/F18PointA/setActivity 5640000. Bq  
/gate/source/F18PointA/gps/particle e+  
/gate/source/F18PointA/setForcedUnstableFlag true  
/gate/source/F18PointA/setForcedHalfLife 6586 s  
/gate/source/F18PointA/gps/energytype Fluor18  
/gate/source/F18PointA/gps/angtype iso  
/gate/source/F18PointA/gps/type Volume  
/gate/source/F18PointA/gps/shape Sphere  
/gate/source/F18PointA/gps/radius 12.5 mm  
/gate/source/F18PointA/gps/centre 0.85 0.85 0.85 cm
```

```
/gate/source/addSource F18PointB  
/gate/source/F18PointB/setActivity 2030000. Bq  
/gate/source/F18PointB/gps/particle e+  
/gate/source/F18PointB/setForcedUnstableFlag true  
/gate/source/F18PointB/setForcedHalfLife 6586 s  
/gate/source/F18PointB/gps/energytype Fluor18  
/gate/source/F18PointB/gps/angtype iso  
/gate/source/F18PointB/gps/type Volume  
/gate/source/F18PointB/gps/shape Sphere  
/gate/source/F18PointB/gps/radius 9. mm  
/gate/source/F18PointB/gps/centre 0.85 -0.85 -0.85 cm
```

```
/gate/source/addSource F18PointC  
/gate/source/F18PointC/setActivity 1160000. Bq  
/gate/source/F18PointC/gps/particle e+  
/gate/source/F18PointC/setForcedUnstableFlag true  
/gate/source/F18PointC/setForcedHalfLife 6586 s  
/gate/source/F18PointC/gps/energytype Fluor18  
/gate/source/F18PointC/gps/angtype iso  
/gate/source/F18PointC/gps/type Volume  
/gate/source/F18PointC/gps/shape Sphere  
/gate/source/F18PointC/gps/radius 8. mm  
/gate/source/F18PointC/gps/centre -0.85 -0.85 0.85 cm
```

```
/gate/source/addSource F18PointD  
/gate/source/F18PointD/setActivity 590000. Bq  
/gate/source/F18PointD/gps/particle e+  
/gate/source/F18PointD/setForcedUnstableFlag true  
/gate/source/F18PointD/setForcedHalfLife 6586 s  
/gate/source/F18PointD/gps/energytype Fluor18  
/gate/source/F18PointD/gps/angtype iso  
/gate/source/F18PointD/gps/type Volume  
/gate/source/F18PointD/gps/shape Sphere  
/gate/source/F18PointD/gps/radius 6.5 mm  
/gate/source/F18PointD/gps/centre -0.85 0.85 -0.85 cm
```

```
/gate/source/list
```



# GATE Configuration

## Physics Descriptor Macro

```
# EM PROCESS
/gate/physics/gamma/selectRayleigh lowenergy
/gate/physics/gamma/selectPhotoelectric lowenergy
/gate/physics/gamma/selectCompton lowenergy

# INACTIVE SECONDARY ELECTRONS
/gate/physics/setElectronCut 1. m

# INACTIVE X-RAYS
/gate/physics/setXRayCut 1. GeV
/gate/physics/setDeltaRayCut 1. GeV
```



# GATE Configuration

## Jazczack Phantom Descriptor Macro

```
/gate/world/daughters/name phantomA  
/gate/world/daughters/insert sphere  
/gate/phantomA/setMaterial Water  
#/gate/phantomA/vis/forceWireframe  
/gate/phantomA/vis/setColor green  
/gate/phantomA/geometry/setRmax 12.5 mm  
/gate/phantomA/placement/setTranslation 0.85 0.85 0.85 cm  
/gate/phantomA/attachPhantomSD
```

```
/gate/world/daughters/name phantomB  
/gate/world/daughters/insert sphere  
/gate/phantomB/setMaterial Water  
#/gate/phantomB/vis/forceWireframe  
/gate/phantomB/vis/setColor green  
/gate/phantomB/geometry/setRmax 9. mm  
/gate/phantomB/placement/setTranslation 0.85 -0.85 -0.85 cm  
/gate/phantomB/attachPhantomSD
```

```
/gate/world/daughters/name phantomC  
/gate/world/daughters/insert sphere  
/gate/phantomC/setMaterial Water  
#/gate/phantomC/vis/forceWireframe  
/gate/phantomC/vis/setColor green  
/gate/phantomC/geometry/setRmax 8. mm  
/gate/phantomC/placement/setTranslation -0.85 -0.85 0.85 cm  
/gate/phantomC/attachPhantomSD
```

```
/gate/world/daughters/name phantomD  
/gate/world/daughters/insert sphere  
/gate/phantomD/setMaterial Water  
#/gate/phantomD/vis/forceWireframe  
/gate/phantomD/vis/setColor green  
/gate/phantomD/geometry/setRmax 6.5 mm  
/gate/phantomD/placement/setTranslation -0.85 0.85 -0.85 cm  
/gate/phantomD/attachPhantomSD
```



# GATE Configuration

## Scanner Descriptor Macro

```
/control/verbose 0
```

```
# WORLD
```

```
/gate/world/geometry/setXLength 2.0 m  
/gate/world/geometry/setYLength 2.0 m  
/gate/world/geometry/setZLength 2.0 m  
/gate/world/setMaterial Air
```

```
# DETECTOR
```

```
/gate/world/daughters/name cylindricalPET  
/gate/world/daughters/insert cylinder  
/gate/cylindricalPET/setMaterial Air  
/gate/cylindricalPET/geometry/setRmax 52. cm  
/gate/cylindricalPET/geometry/setRmin 28. cm  
/gate/cylindricalPET/geometry/setHeight 24.02 cm  
/gate/cylindricalPET/vis/forceWireframe
```

```
# SHIELDING
```

```
/gate/cylindricalPET/daughters/name Shielding  
/gate/cylindricalPET/daughters/insert cylinder  
/gate/Shielding/setMaterial Lead  
/gate/Shielding/geometry/setRmax 46.132 cm  
/gate/Shielding/geometry/setRmin 28. cm  
/gate/Shielding/geometry/setHeight 2.86 cm  
/gate/Shielding/vis/forceSolid  
/gate/Shielding/vis/forceWireframe  
/gate/Shielding/vis/setColor white
```

```
# REPEAT SHIELDING
```

```
/gate/Shielding/repeaters/insert linear  
/gate/Shielding/linear/setRepeatNumber 2  
/gate/Shielding/linear/setRepeatVector 0. 0. 21.16 cm
```

```
# DETECTOR = RSECTOR
```

```
/gate/cylindricalPET/daughters/name rsector  
/gate/cylindricalPET/daughters/insert box  
/gate/rsector/geometry/setXLength 40 mm  
/gate/rsector/geometry/setYLength 94.5 mm  
/gate/rsector/geometry/setZLength 18.3 cm  
/gate/rsector/setMaterial Glass  
/gate/rsector/placement/setTranslation 45.2 0 0 cm  
/gate/rsector/vis/forceWireframe
```

```
# CRYSTAL
```

```
/gate/module/daughters/name crystal  
/gate/module/daughters/insert box  
/gate/crystal/geometry/setXLength 20. mm  
/gate/crystal/geometry/setYLength 4 mm  
/gate/crystal/geometry/setZLength 6 mm  
/gate/crystal/setMaterial GSO  
/gate/crystal/placement/setTranslation 0 0 0 mm
```

```
# LAYER GSO
```

```
/gate/crystal/daughters/name GSO  
/gate/crystal/daughters/insert box  
/gate/GSO/geometry/setXLength 20. mm  
/gate/GSO/geometry/setYLength 4 mm  
/gate/GSO/geometry/setZLength 6 mm  
/gate/GSO/placement/setTranslation 0 0 0 mm  
/gate/GSO/setMaterial GSO
```

```
# REPETITION CRISTAL
```

```
/gate/crystal/repeaters/insert cubicArray  
/gate/crystal/cubicArray/setRepeatNumberX 1  
/gate/crystal/cubicArray/setRepeatNumberY 22  
/gate/crystal/cubicArray/setRepeatNumberZ 29  
/gate/crystal/cubicArray/setRepeatVector 0. 4.3 6.3 mm
```

```
# REPETITION RSECTOR
```

```
/gate/rsector/repeaters/insert ring  
/gate/rsector/ring/setRepeatNumber 28
```

```
# PHANTOM
```

```
# The phantom must model the attenuation geometry  
/gate/world/daughters/name phantom  
/gate/world/daughters/insert cylinder  
/gate/phantom/geometry/setRmax 25 cm  
/gate/phantom/geometry/setHeight 18.5 cm  
/gate/phantom/placement/setTranslation 0. 0. 0. cm  
/gate/phantom/setMaterial Water
```

```
# ATTACH SYSTEM
```

```
/gate/systems/cylindricalPET/rsector/attach rsector  
/gate/systems/cylindricalPET/module/attach module  
/gate/systems/cylindricalPET/crystal/attach crystal  
/gate/systems/cylindricalPET/layer0/attach GSO
```

```
# ATTACH LAYER SD
```

```
/gate/GSO/attachCrystalSD  
/gate/rsector/attachPhantomSD  
/gate/module/attachPhantomSD  
/gate/phantom/attachPhantomSD  
#/gate/Shielding/attachPhantomSD
```



# Methods

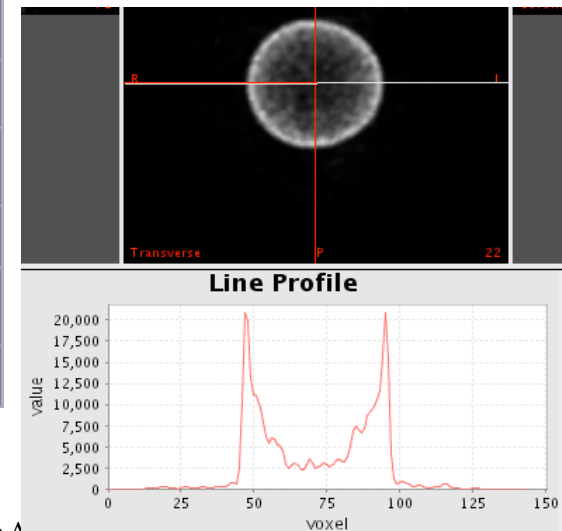
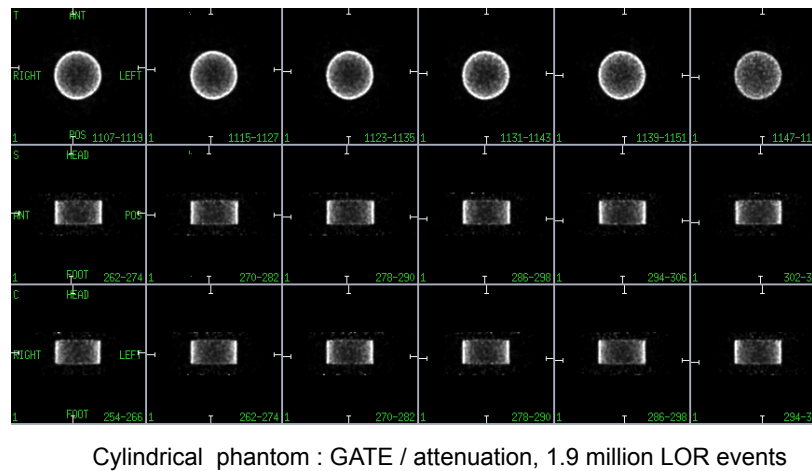
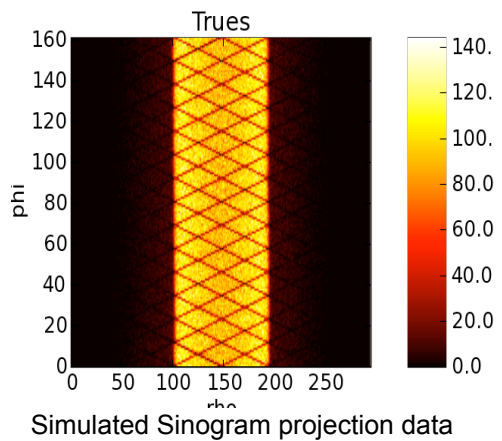
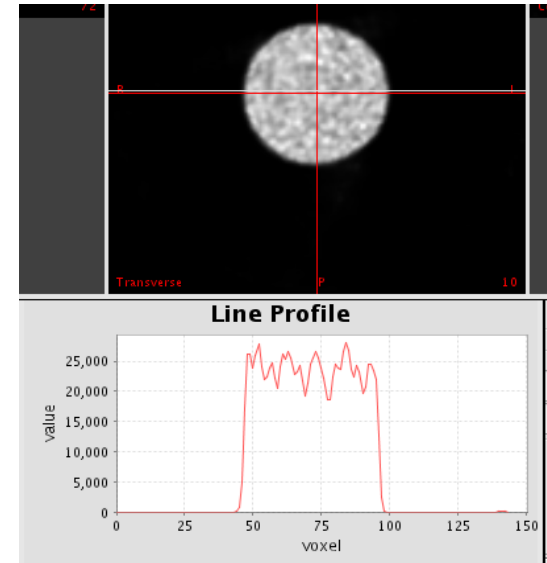
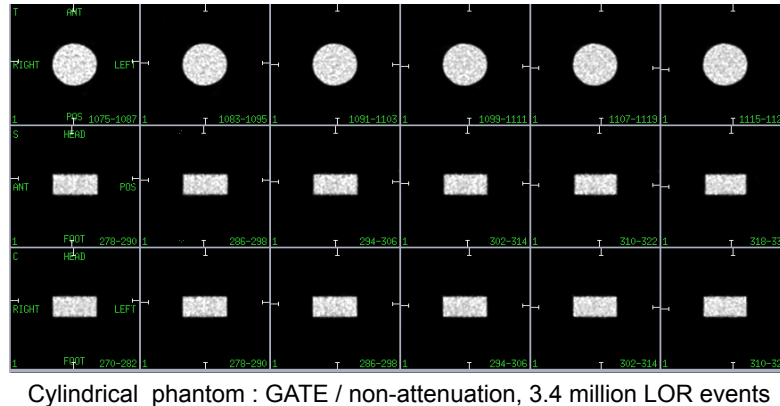
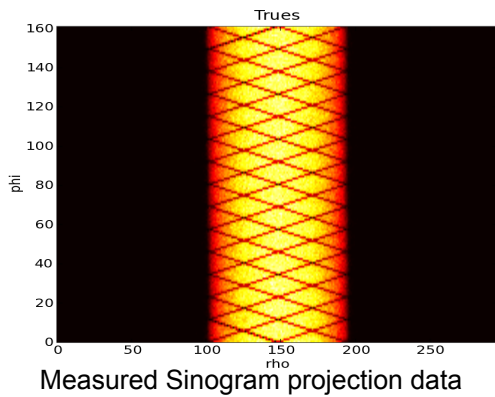
- 37 MBq in FOV
- Single CPU simulation
  - 1 second simulation
    - 1 day for geometric phantom
    - 3 day for voxelised phantom
- 5 second breathing cycle
  - 25 frames
  - 200 msec respiratory frames



# GATE Validation

## Geometric phantoms

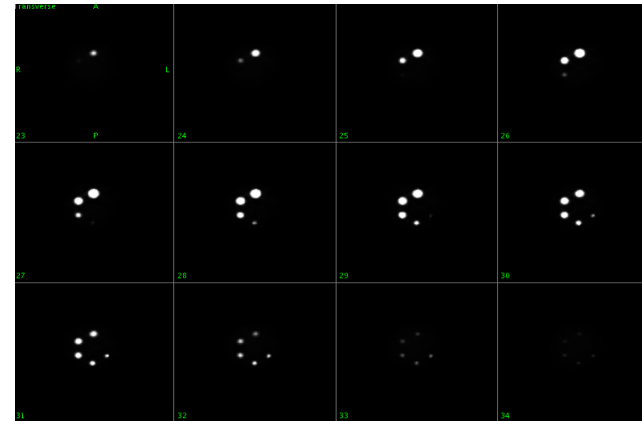
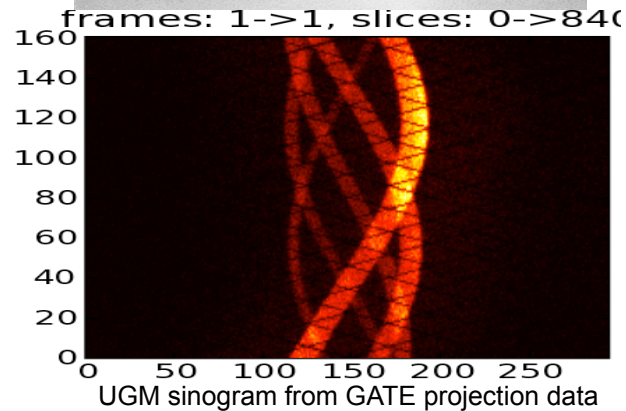
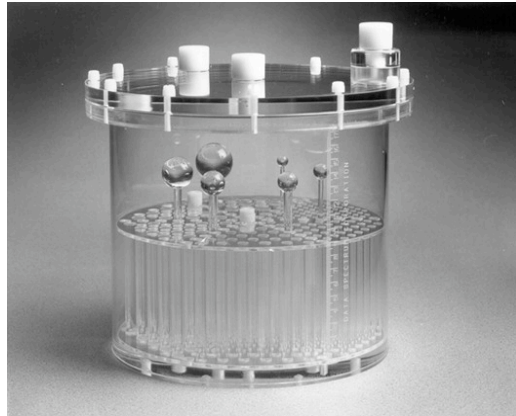
- Cylindrical phantom uniform simulation



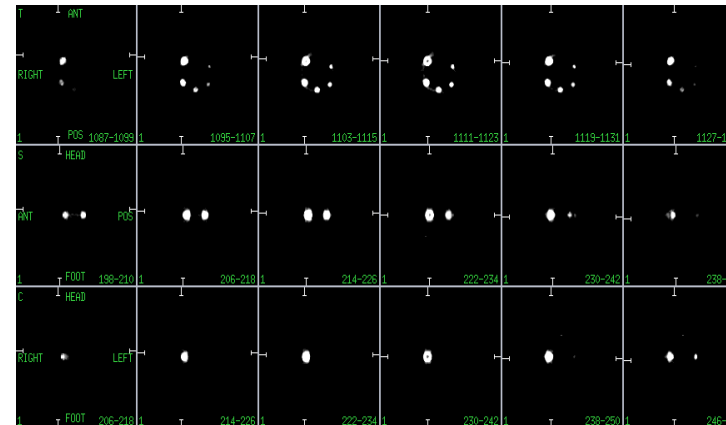
# GATE Validation

## Geometric Phantoms

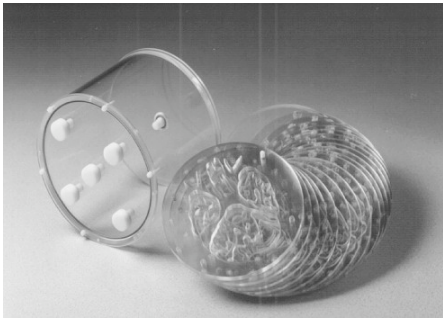
- Five sphere sources in Jaszczack phantom simulation



Jaszczack phantom measurement by Allegro PET with 300 million line of response (LOR) events

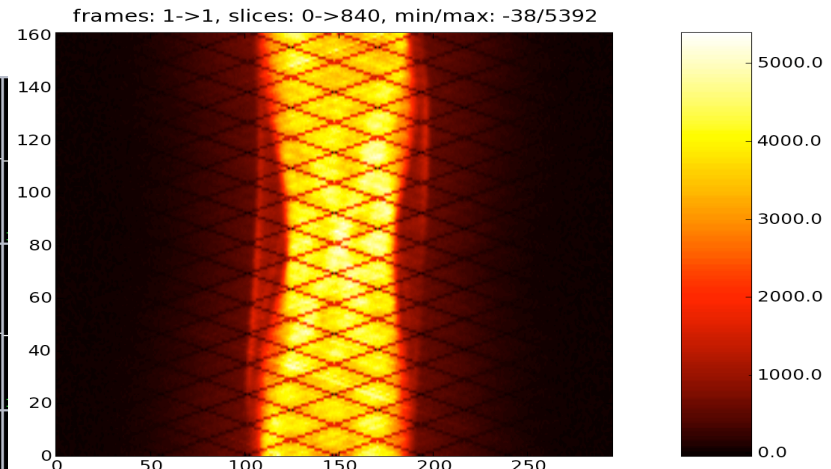
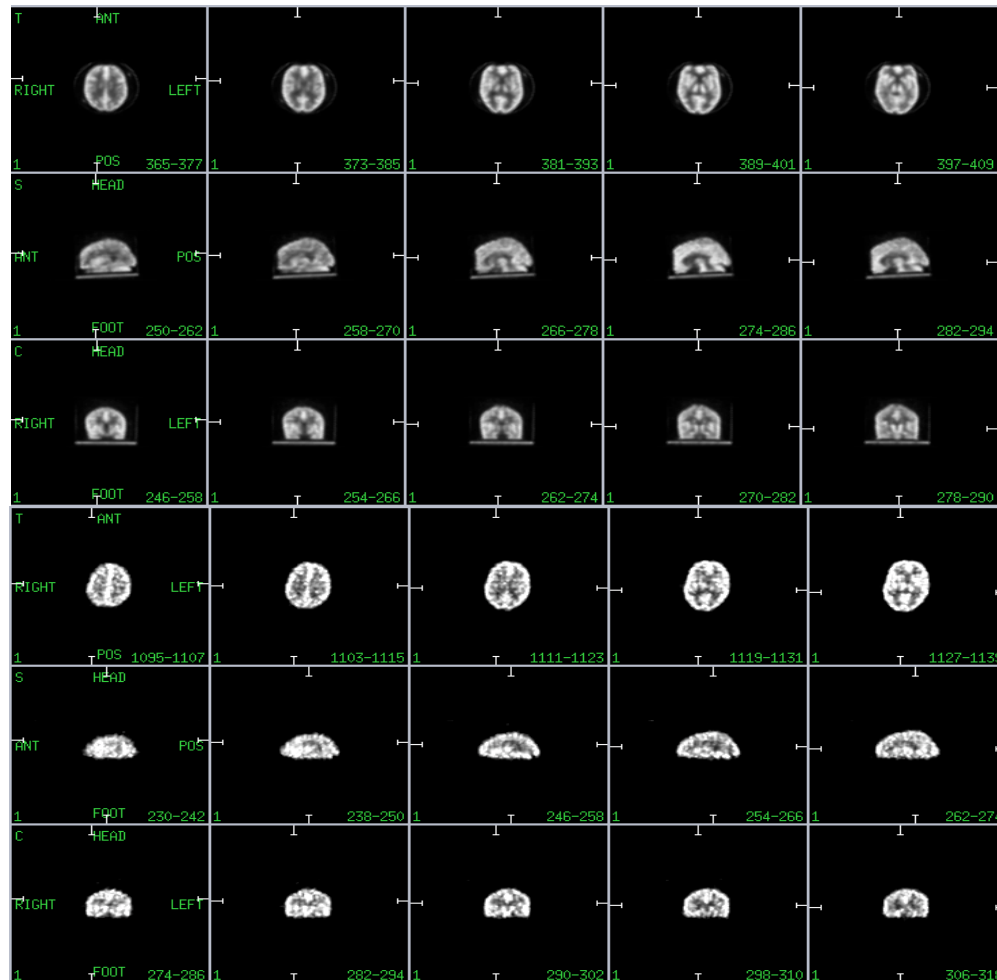


Simulation reconstructed image with 3 million LOR events

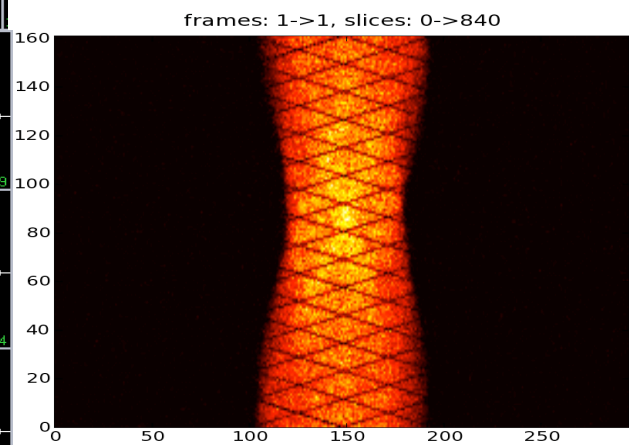


# GATE Validation

## Voxelised Hoffman Phantom



Hoffman phantom measured by Allegro  
51 million LOR events

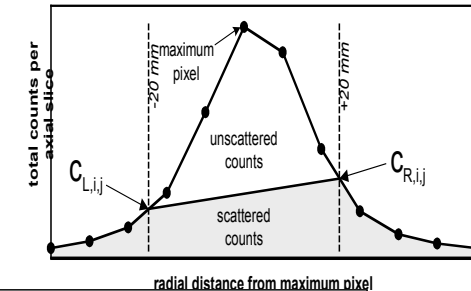
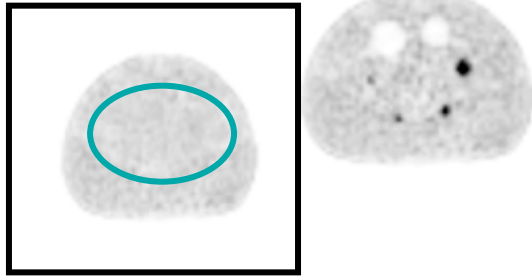


Hoffman phantom simulated by GATE w/o attenuation  
0.89 million LOR events

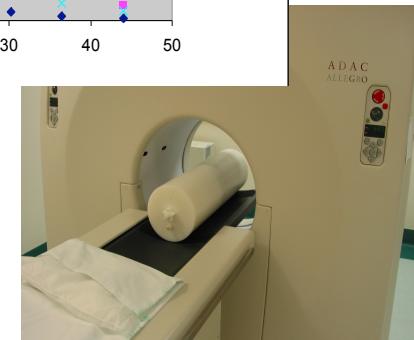
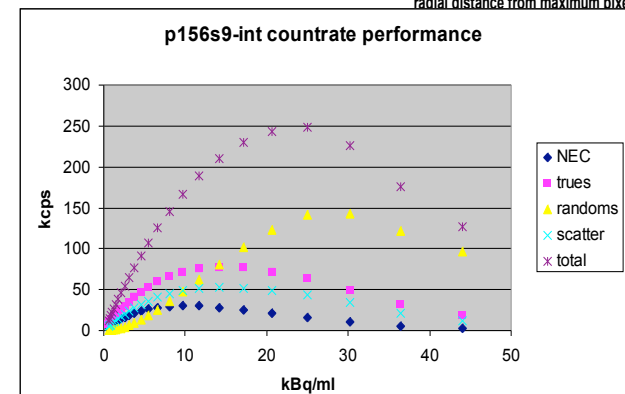


# NEMA-NU2

## Acceptance Testing



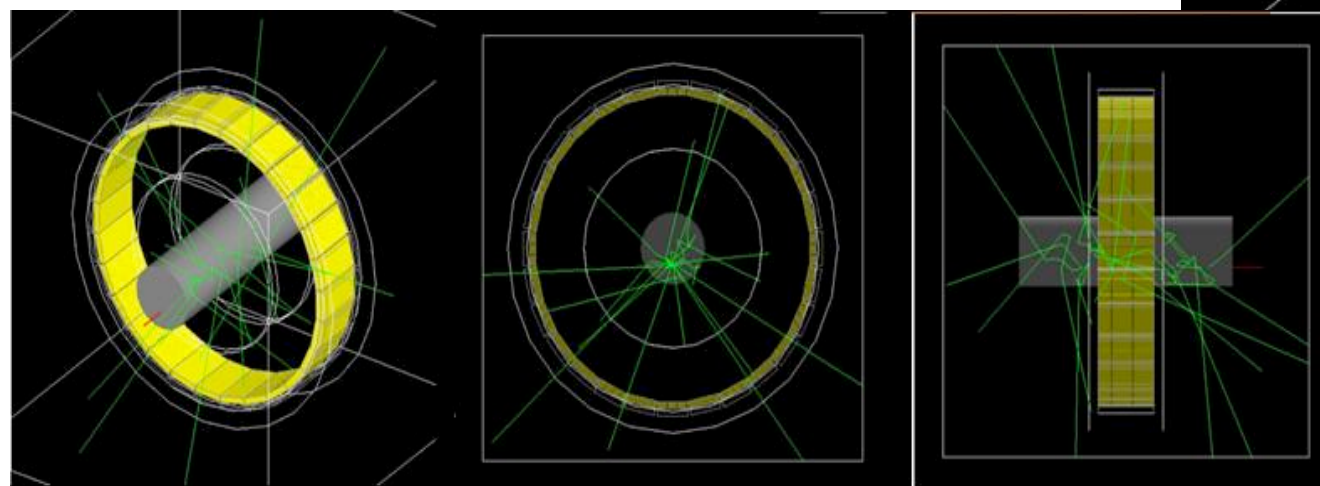
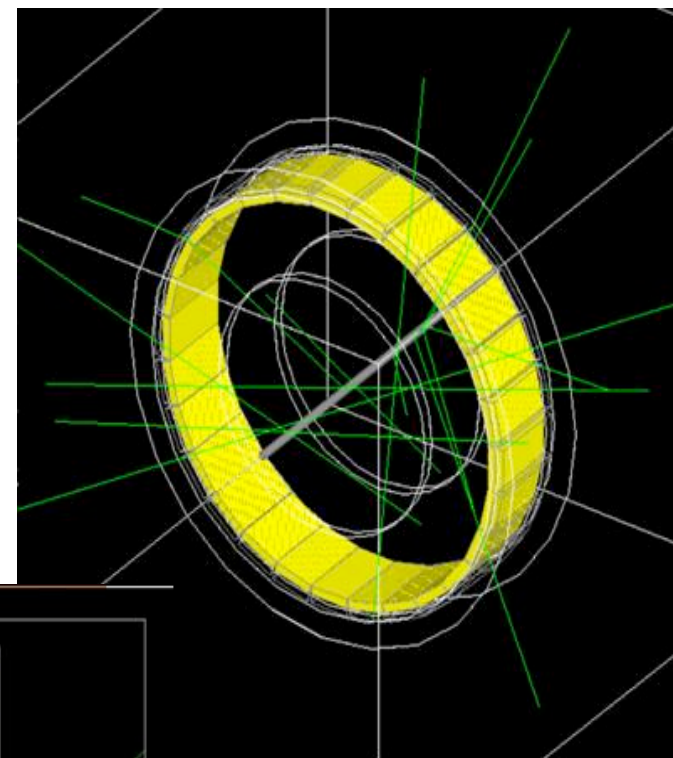
- Spatial Resolution
- Scatter Fraction
- Countrate Losses
- Randoms Measurement
- Sensitivity
- Corrections
- Image Quality
- Accuracy of Attenuation/Scatter corrections



# NEMA-NU2

## Software Validation

- Phantom specification
  - Sensitivity
  - Countloss
  - Image Quality



# Respiratory Motion

- Simulate respiratory motion in PET
  - Develop data-driven motion detection schemes
  - Validate motion correction schemes
- GATE 2.2.0
  - GEANT4 Application for Tomographie Emission
- Phantoms
  - Geometric phantom validation
  - Voxelised phantom validation
    - NCAT: NURBS Based Cardiac Torso

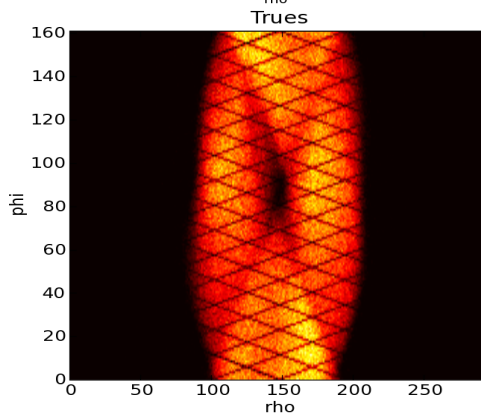
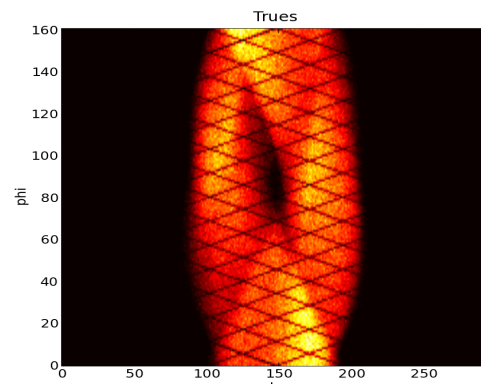


# Respiratory Motion

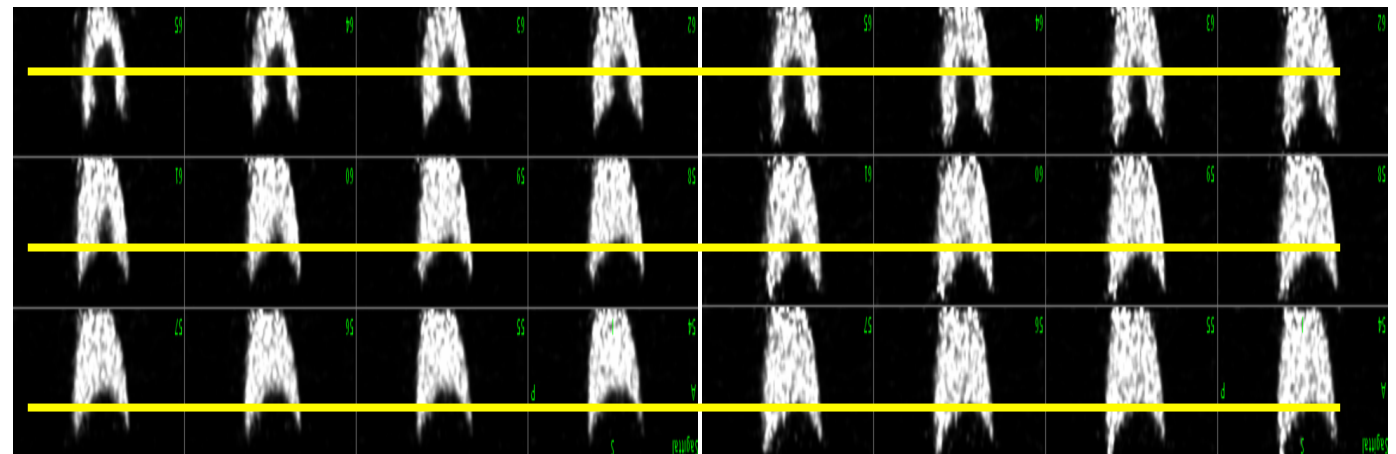
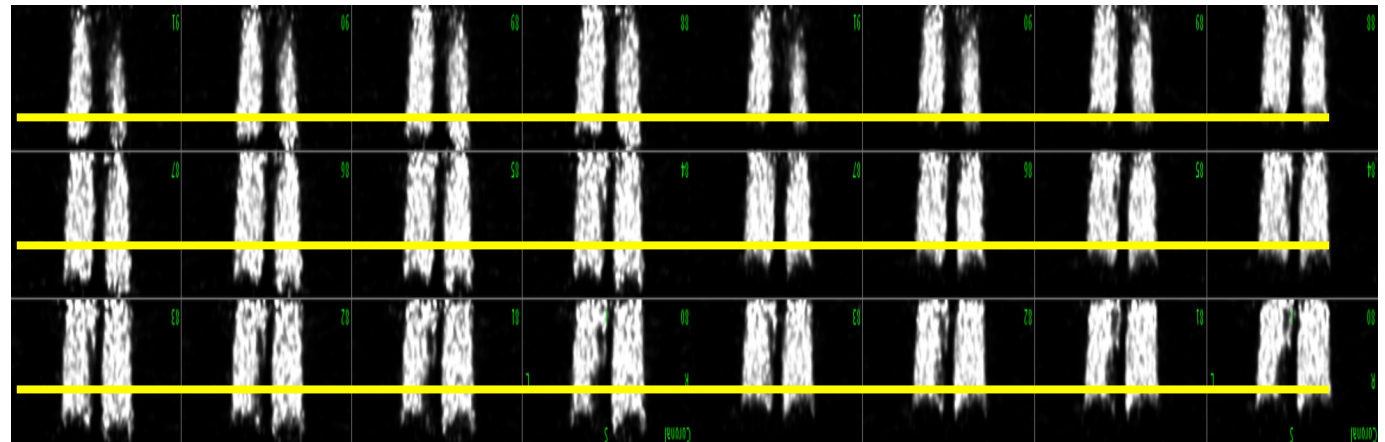
## Voxelised Phantom

- **Simulation**

- GATE & 4D-NCAT  
Lung Activity  
w/o attenuation



1<sup>st</sup> and 12<sup>th</sup> Sinogram frame



1<sup>st</sup> frame sagittal image

12<sup>th</sup> frame sagittal image

1<sup>st</sup> frame for expiration with non-attenuation modelled, 1 million LOR events and comparison with the 12<sup>th</sup> inspiration frame



Austin Health

# Respiratory Motion

## Voxelised Phantom

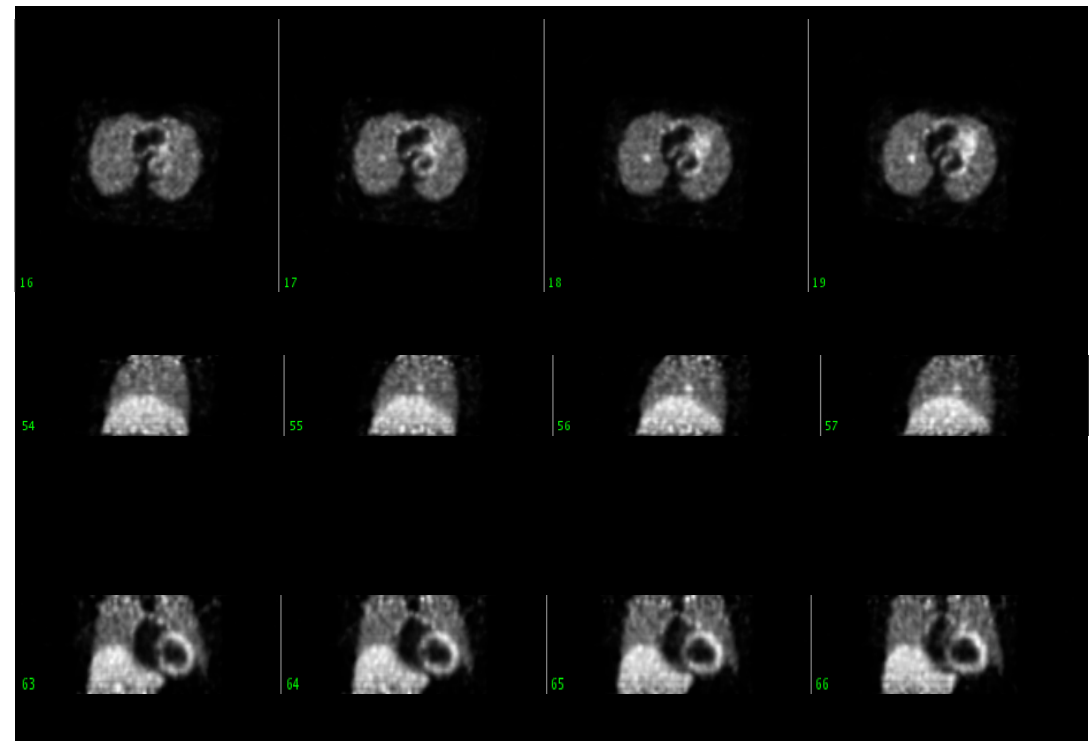
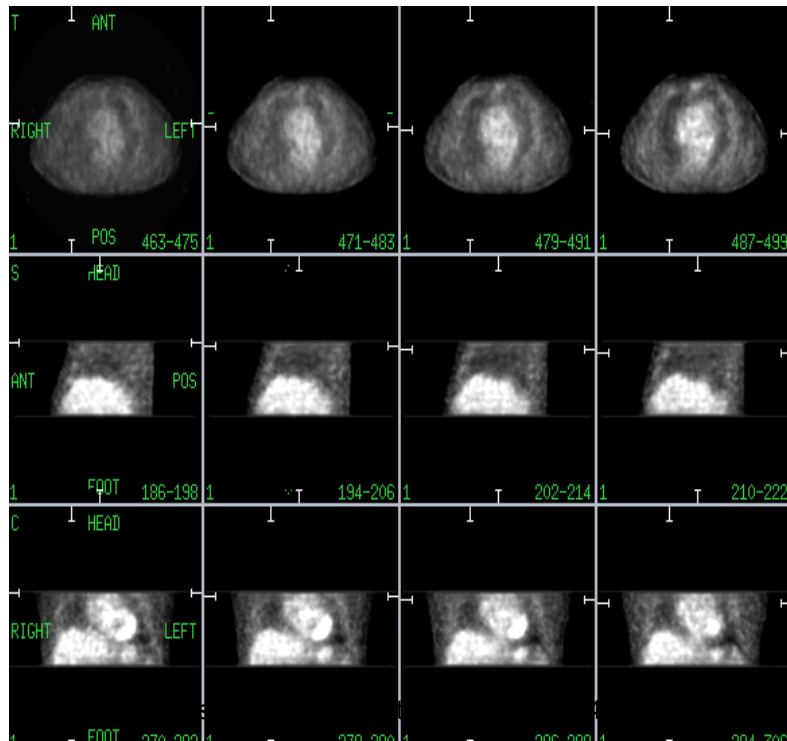
- **Simulation**

- GATE & 4D-NCAT

Clinically Realistic Activities (no mediastinum)

Lung Lesion

w/o Attenuation Modelling



Simulation reconstructed image, 8.8 millions LORs



Austin Health

# Respiratory Motion

## Simulation times (2.2.0)

Summary of simulations			Coincident Rate ( kcps )	Computational / Measurement Times		
Classification	phantoms	Simulations / Measurements		Measured	Compute	LOR events
<b>Geometric</b> phantom & source	Jaszczsak	Measurement with attenuation by Allegro	166	30 minus	n/a	<u>Non Attenuation:</u> 1 million/4 hrs
		Simulation with attenuation	517	5.8 sec	4.4 days	
	Cylinder	Simulation without attenuation	106	3.2 sec	1 day	
		Simulation with attenuation	311	6.1 sec	3 days	<u>Attenuation:</u> 1 million/5 days
<b>Voxelised</b> phantom & source	Hoffman	Measurement with attenuation by Allegro	170	30 sec	n/a	<u>Non Attenuation:</u> 1 million/4hrs
		Simulation without attenuation	262	6.1 sec	10 hours	
		Simulation with attenuation	262	6.1 sec	12 days	<u>Attenuation:</u> 1 million/8 days
	NCAT	Measurement with attenuation by Allegro	113	5 mins	n/a	<u>Non Attenuation:</u> 1 million/5 hrs
		Simulation with attenuation, heart, liver	120	10 sec	24 days	
		1 <sup>st</sup> frame simulation without attenuation	227	4.4 sec	2 days	
		12 <sup>th</sup> frame simulation without attenuation	302	2.9 sec	2 days	<u>Attenuation:</u> 1 million/24 days
		Average frame simulation without attenuation	270	3.7 sec	2 days	
		1 <sup>st</sup> frame simulation with attenuation	264	2.27 sec	24 days	
		1 <sup>st</sup> frame simulation with a lesion	733	12 sec	2 days	



# Respiratory Motion

## Simulation Evaluation Summary

- **Voxelised vs Geometric**
  - Up to a factor of 5 slower
  - Dependent on size of voxelised phantom
- **Attenuation vs Non-Attenuation modelling**
  - Up to a factor of 50 slower
- **Supercomputing facilities**
  - VPAC (Brecca: 180 CPU Linux Cluster)
  - Spawn individual frames

GATE and 4D-NCAT are able to provide practical phantom listmode data and lung voxelised phantom respectively.

Simulations provide a valuable tool for the modelling of respiratory motion.



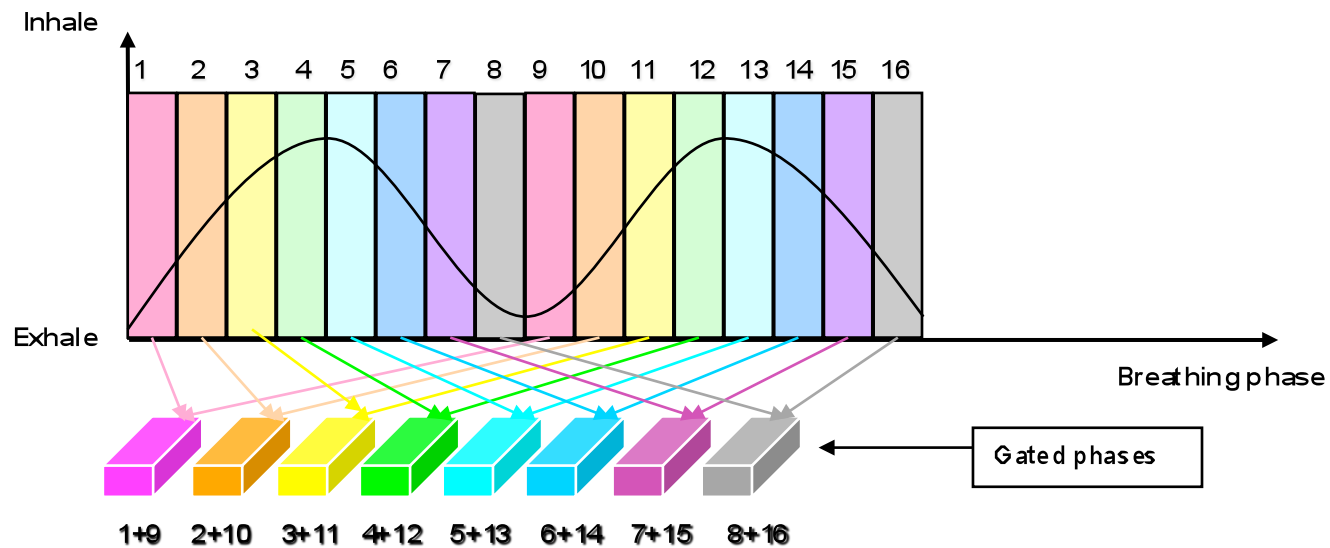
# Respiratory Gating

- Gating techniques
  - Detect Phase of Motion
    - Hardware, Data-driven
  - Image at nominated Phase
- Correction techniques
  - Gated images translated reference phase

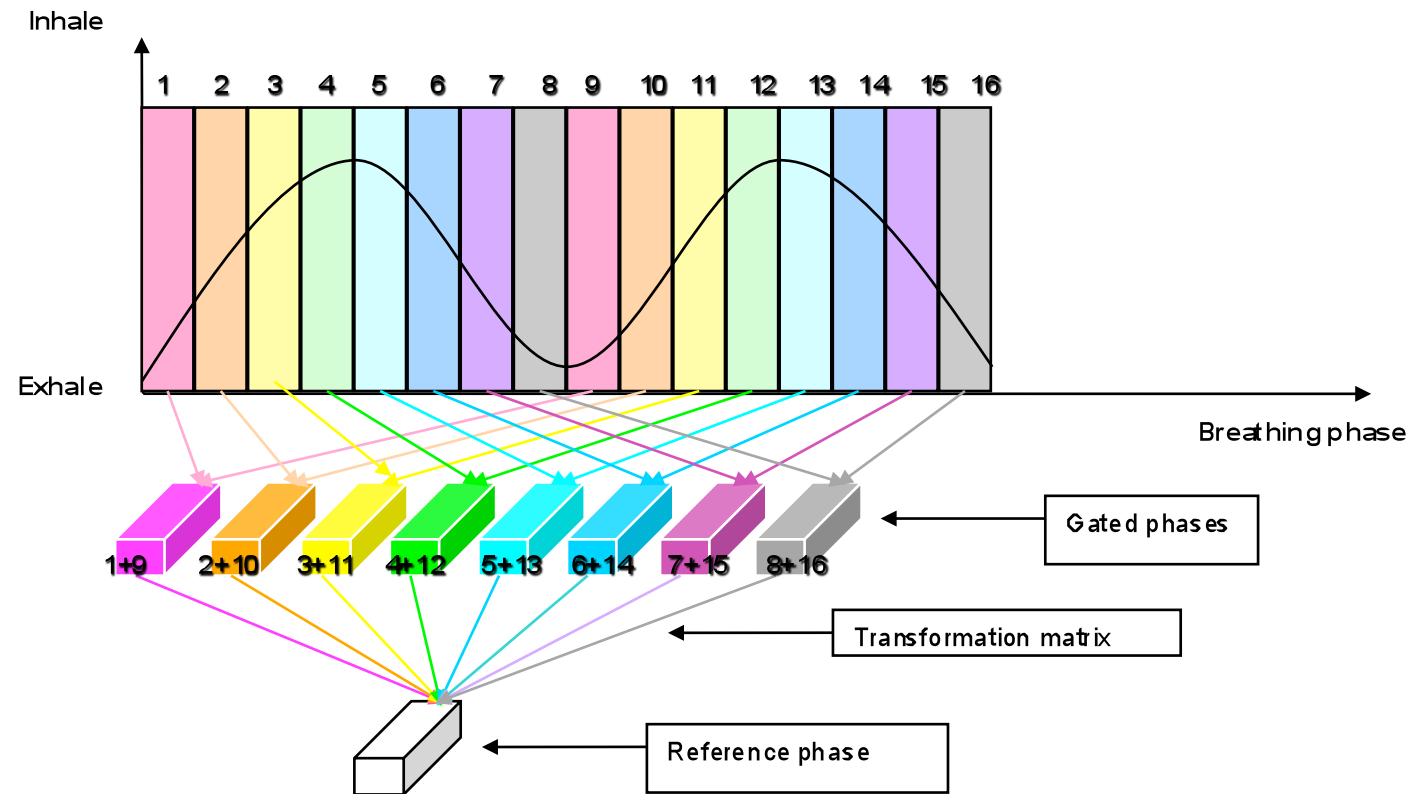


# Respiratory Gating

Two breathing cycles for gating procedure. These two breathing cycles can be gated into 8 phases.



# Respiratory Correction

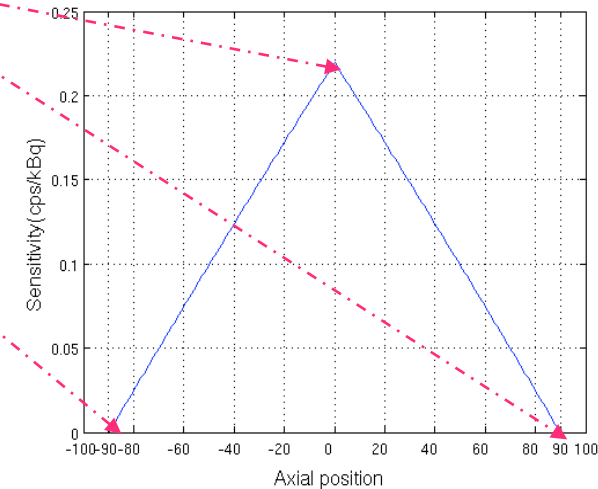
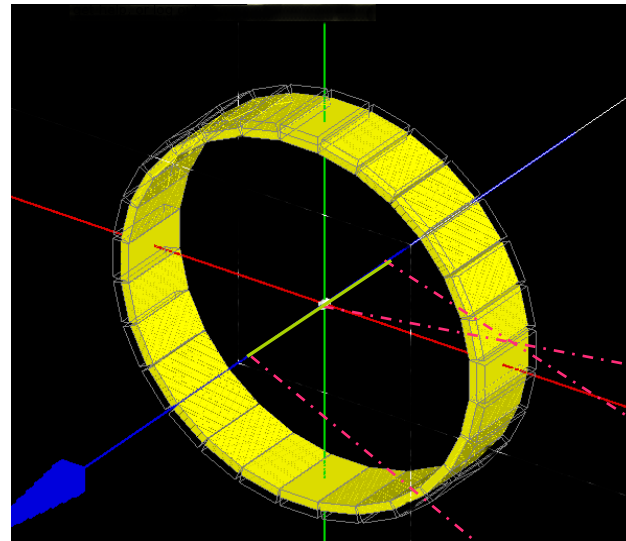


Two breathing cycles are gated into 8 breathing phases, which can be translated into the reference phase with transformation matrix.



# Motion Detection

Philips Allegro Scanner, the geometric sensitivity of 3D PET cylindrical scanner varies with the axial position. The sensitivity value is the highest at the centre of FOV while the sensitivity value at the edge of FOV is close zero.

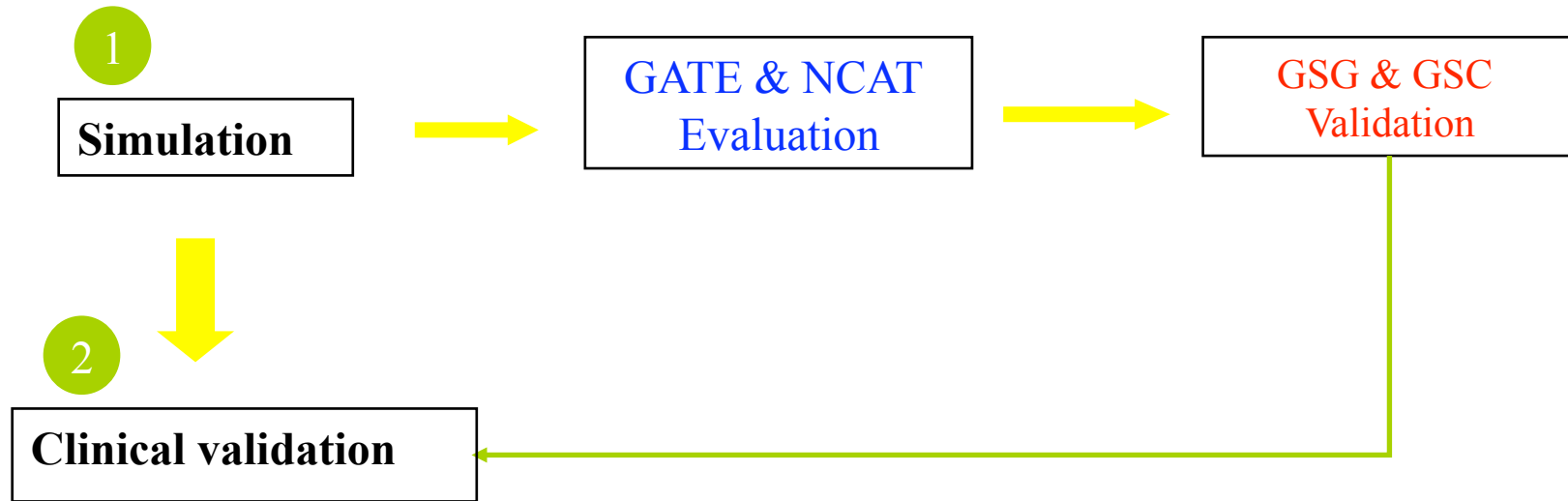


Respiratory motion compensation in PET imaging could be implemented in terms of the geometric sensitivity along axis of the scanner.



# Respiratory Motion

## Geometric Sensitivity



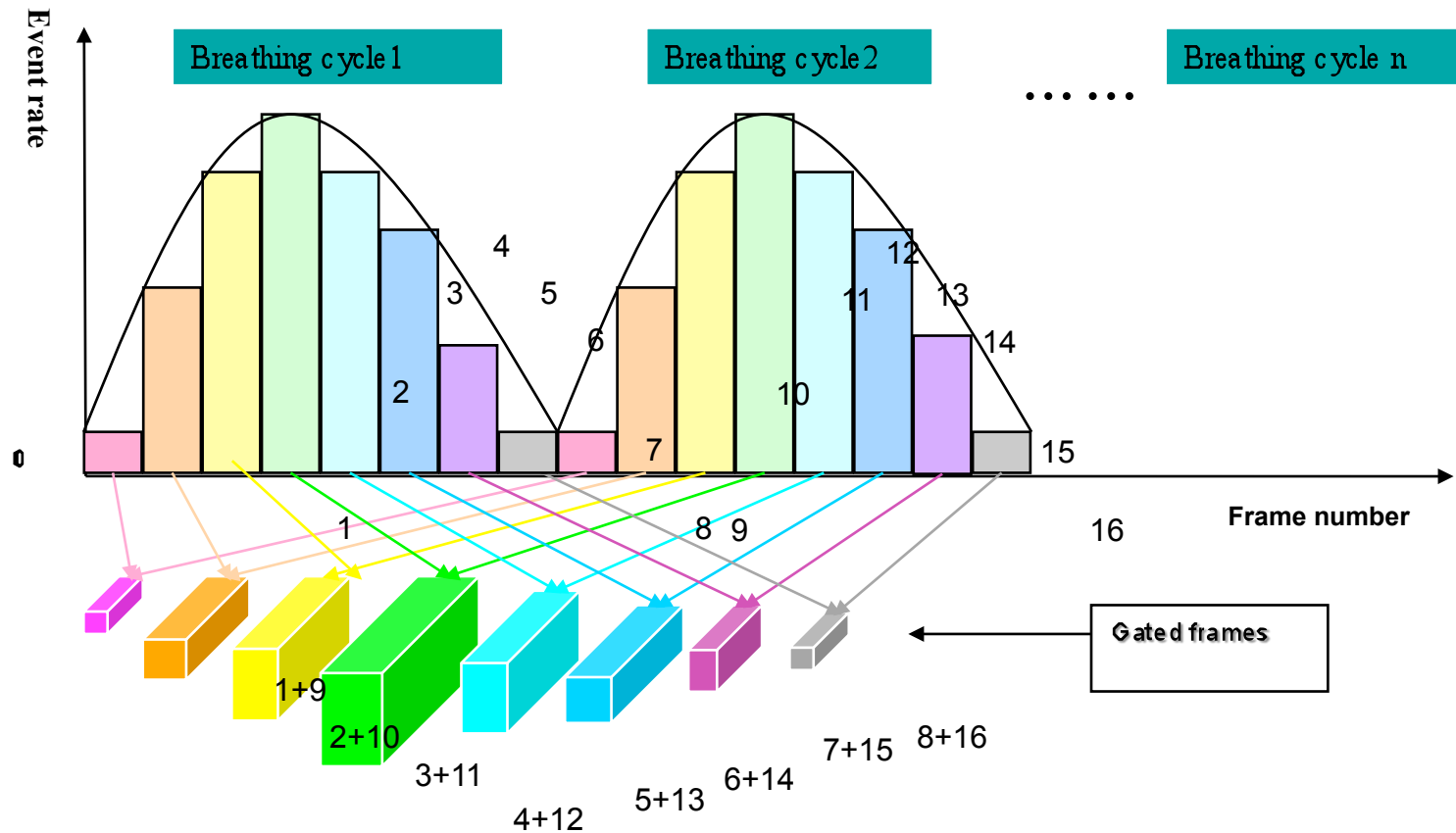
**GSG:** Geometric Sensitivity Gating

**GSC:** Geometric Sensitivity Correction



# Respiratory Motion

## Geometric Sensitivity Gating

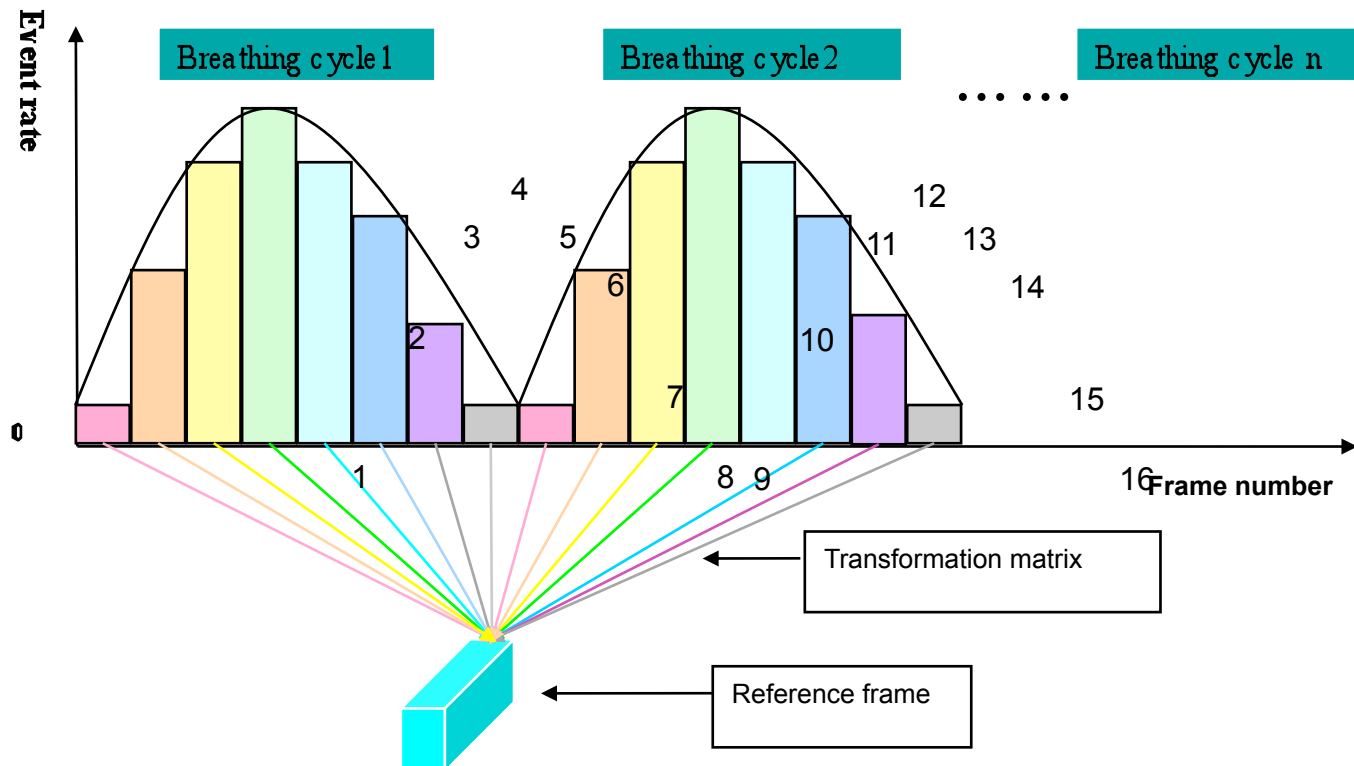


The cyclic change in event-rate with respect to frames illustrating the respiratory breathing cycle. The count-rate in two breathing cycles is used to determine gating-phases. Each cycle is 5 seconds and 8 frames motion along axis.



# Respiratory Motion

## Geometric Sensitivity Gating



The change in event-rate with respect to frames illustrating the respiratory motion displacements. The count-rate in two breathing cycles is used to determine transformation matrix. Each frame is directly moved to the reference frame. Each cycle is 5 seconds with 8 frames motion along axis.



# Respiratory Motion

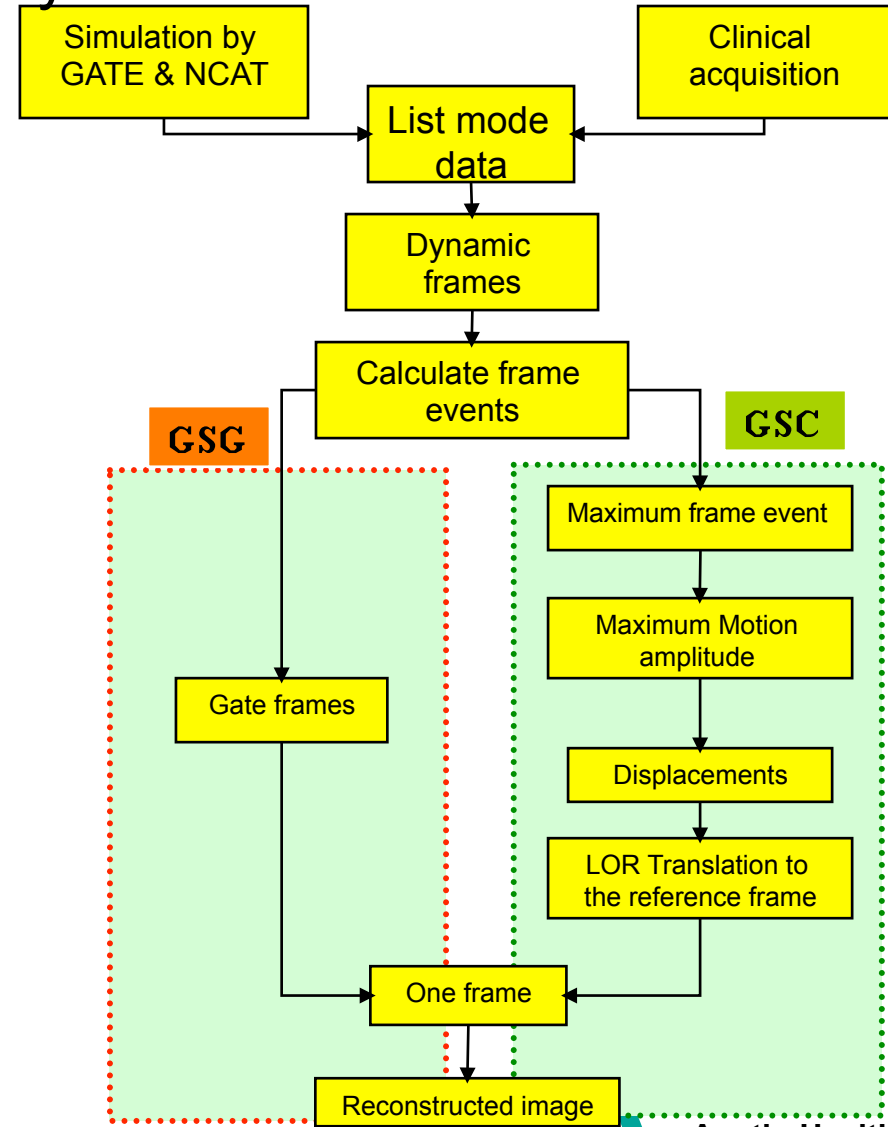
## Geometric Sensitivity Correction

Displacements transformation matrix calculation for GSC:

$$M(i) = \frac{A}{\max(\arcsin(\frac{f_{\max} - f(i)}{f_{\max}}))} * \arcsin(\frac{f_{\max} - f(i)}{f_{\max}})$$

( $i = 1, 2, 3, \dots, n$ )

- $M(i)$  : Transformation matrix
- $i$  : Frame number
- $A$  : Maximum motion amplitude
- $f_{\max}$  : Maximum frame events
- $f(i)$  : Each frame events



8th December, 2008

The summary of implementing Geometrical Sensitivity Gating (GSG) and Geometrical Sensitivity Correction (GSC).



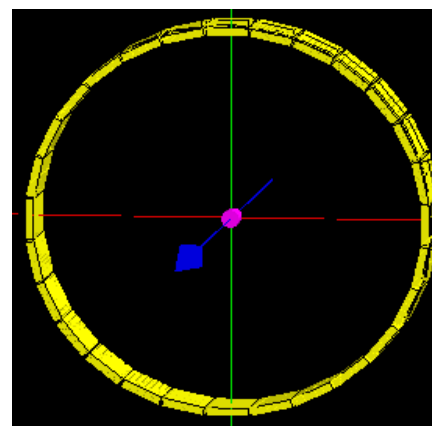
# Respiratory Motion

## Geometric Sensitivity Gating Simulation

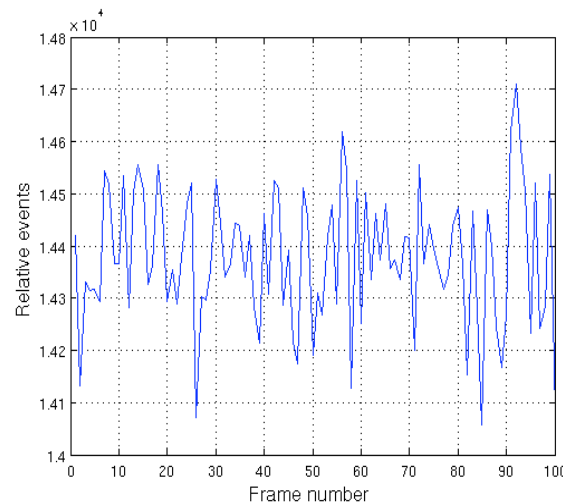
- **Geometric Source**

- **Cylindrical Object**

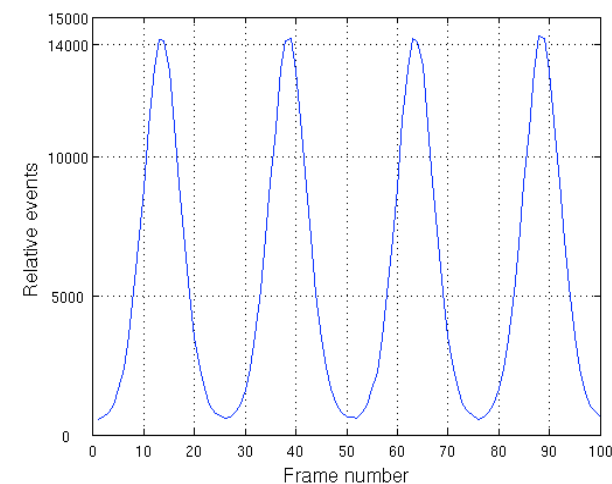
- GATE defined cylindrical phantom
    - 100 frames were generated
    - 2 oscillation cycles over 10sec.



**Static** simulation : 4% variation in event-rate.



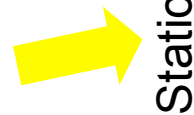
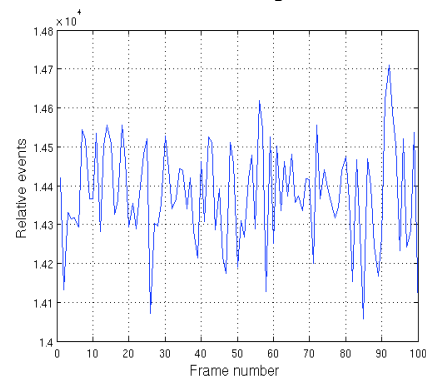
**Motion** simulation : sinusoid nature 96% change



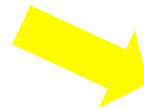
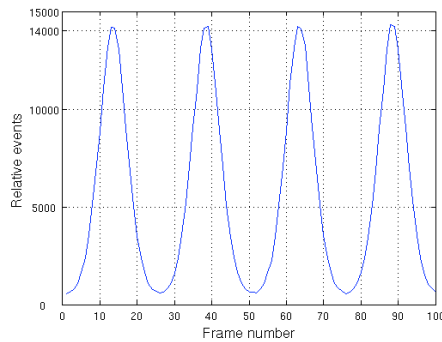
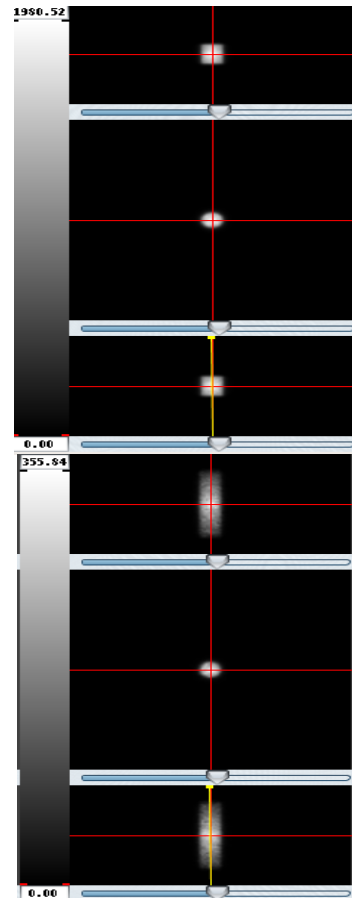
# Respiratory Motion

## Geometric Sensitivity Gating

- GATE defined cylindrical phantom
- 100 frames generated
- 2 oscillation cycles over 10sec.



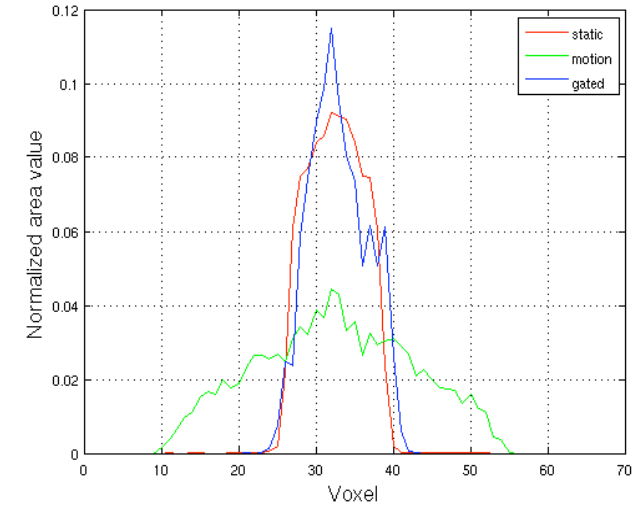
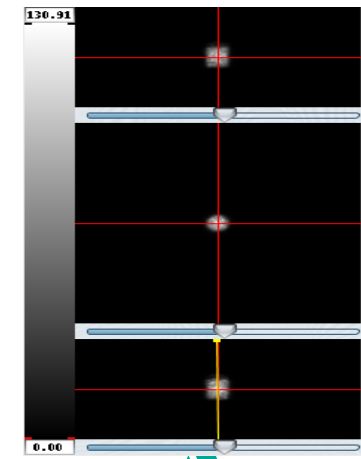
Static



Motion



Gated



Line profile comparison of static, motion and gated.

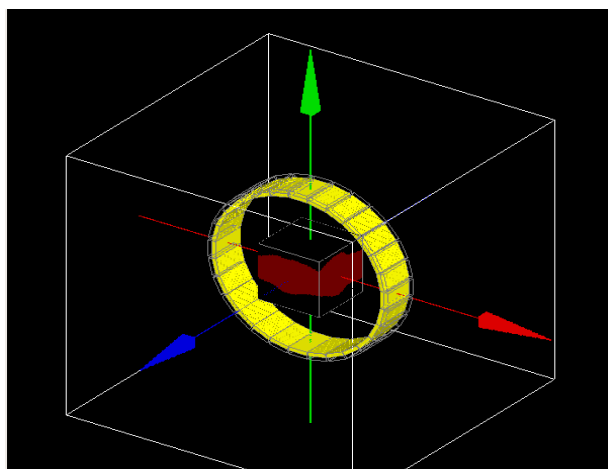
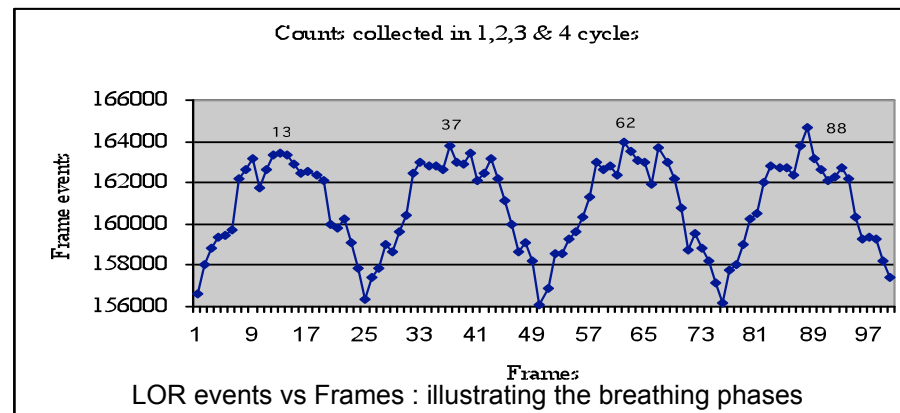
# Respiratory Motion

## Geometric Sensitivity Gating Simulation

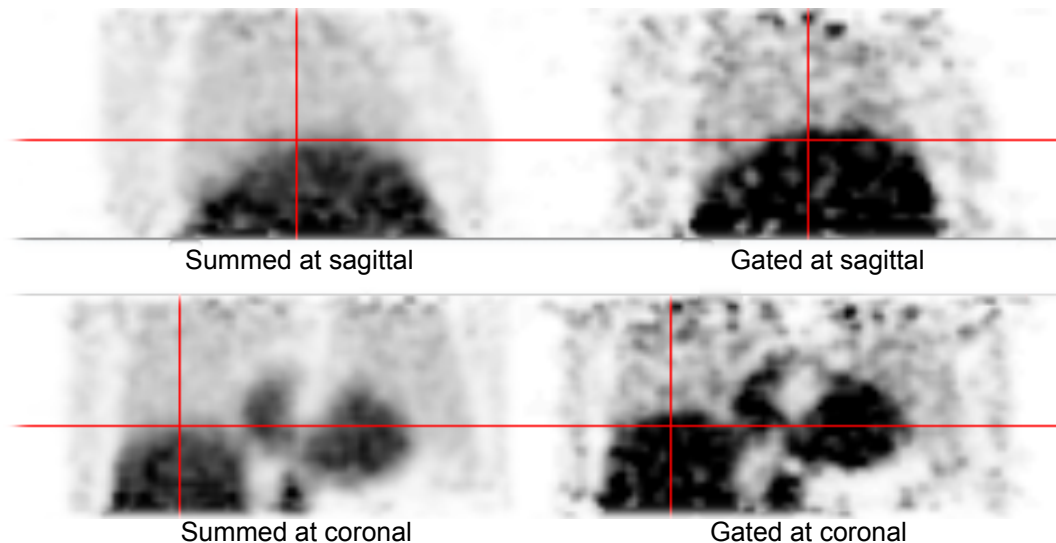
- Voxelised Source**

- 4D NCAT

- No Attenuation Modelling
- 250 frames were generated
- 10 breathing cycles over 50 sec.



64x64x64 matrix of frame with 320mm length was centered in the FOV with 180mm length along Z axis.



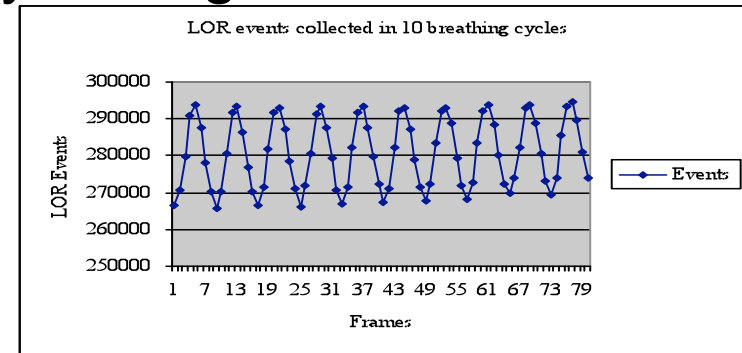
# Respiratory Motion

## Geometric Sensitivity Gating

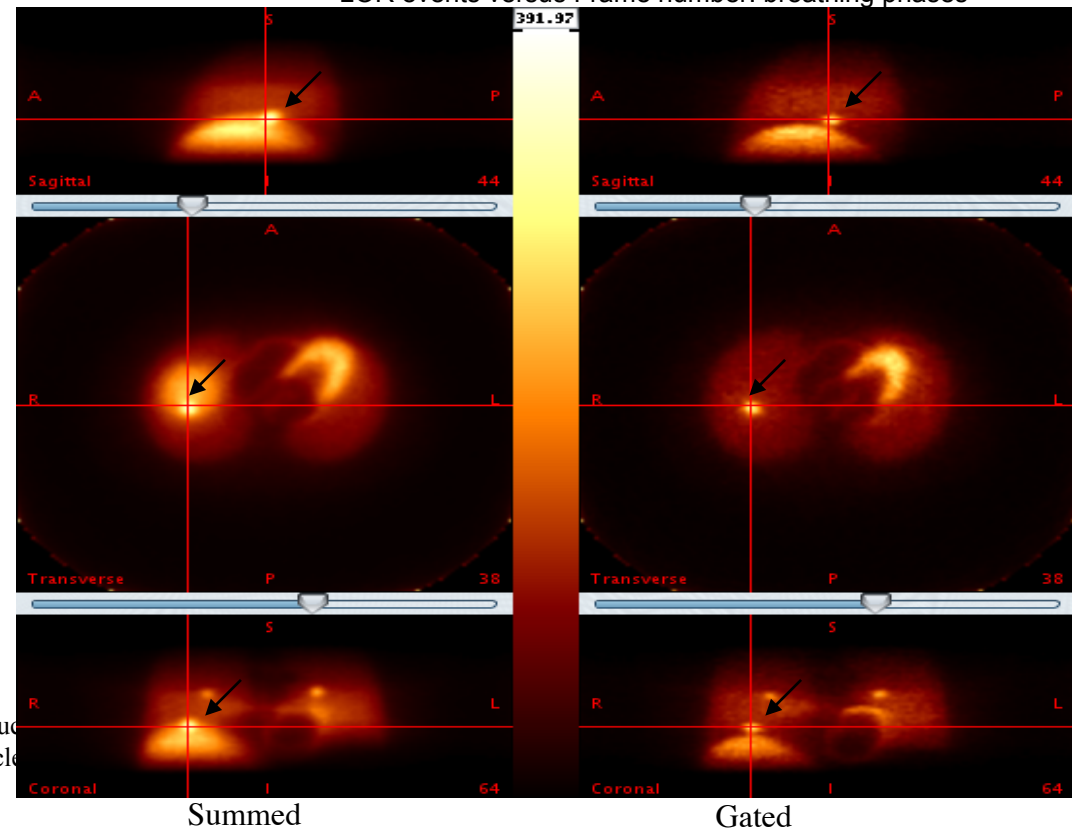
- Voxelised Source

- 4D NCAT

- No Attenuation Modeling
- Lesion
- 80 frames / 10 cycles
- $7.1 \times 10^7$  total
- $3.3 \times 10^7$  gated



LOR events versus Frame number: breathing phases



# Respiratory Motion

## Geometric Sensitivity Gating

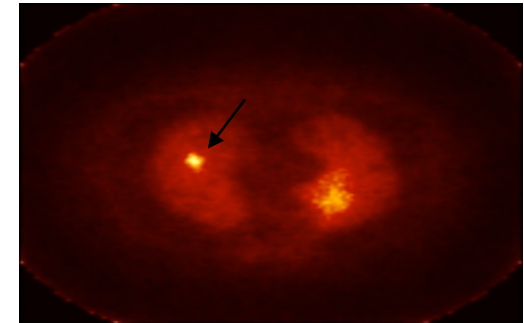
- **Voxelised Source**

- 4D NCAT

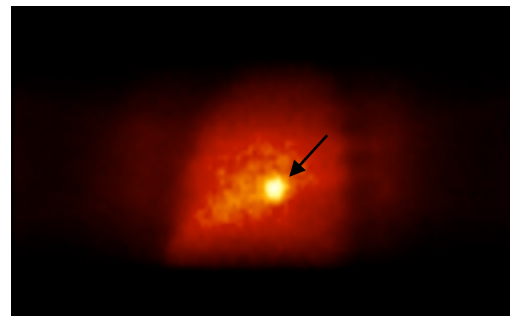
- Attenuation Modeling
- Lesion
- 80 frames / 10 cycles



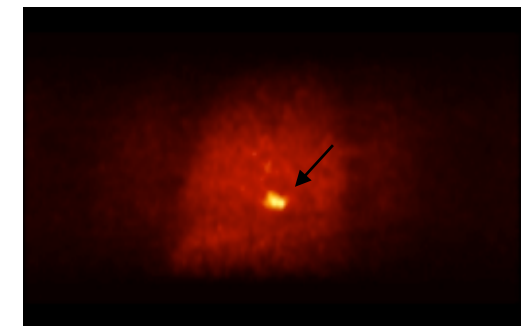
Summed: transaxial



Gated: transaxial



Summed: sagittal



Gated: sagittal

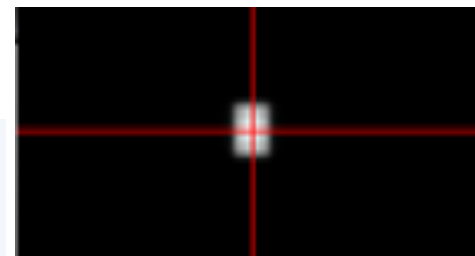
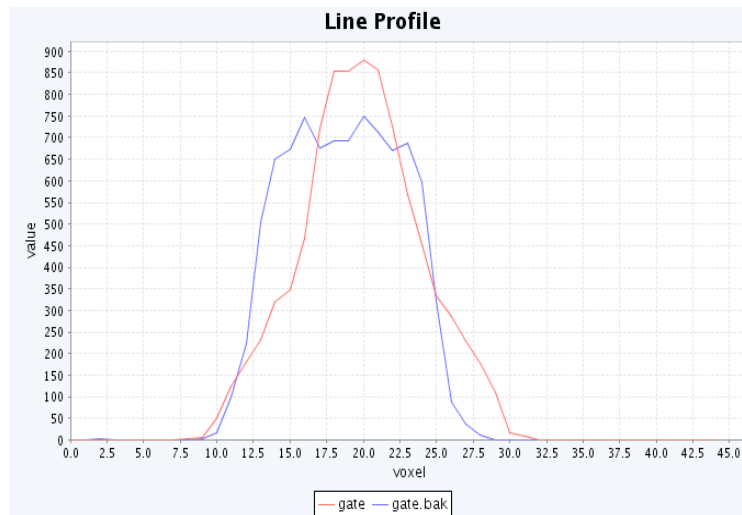
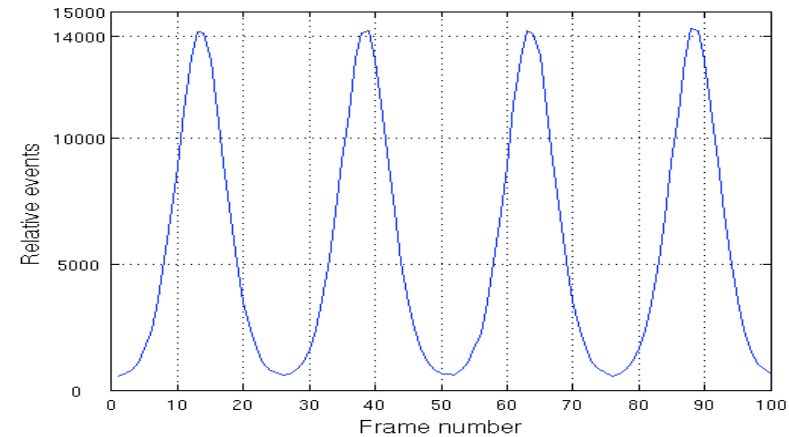
# Respiratory Motion

## Geometric Sensitivity Correction

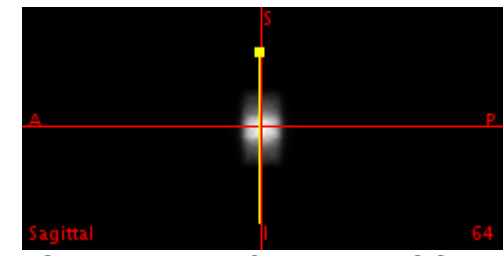
- **Geometric Source**

- **Cylindrical Object**

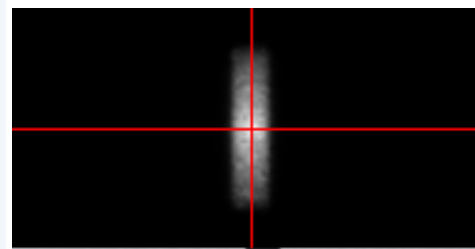
- GATE defined cylindrical phantom
- 5 cm amplitude motion
- 100 frames, 2 cycles over 10 sec
- Corrected by
  - Centre of Mass (COM)
  - GSG respectively.



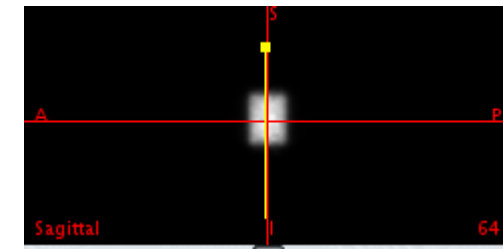
Static



Corrected 100 frames by COM



Motion



corrected 100 frames by GSC

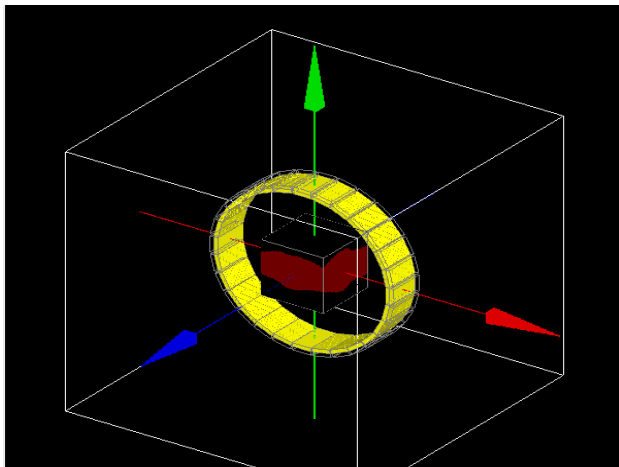
# Respiratory Motion

## Geometric Sensitivity Correction

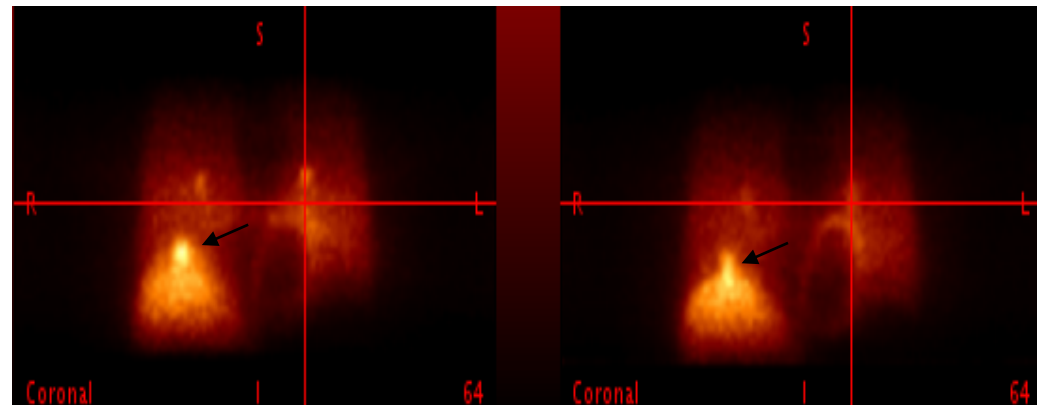
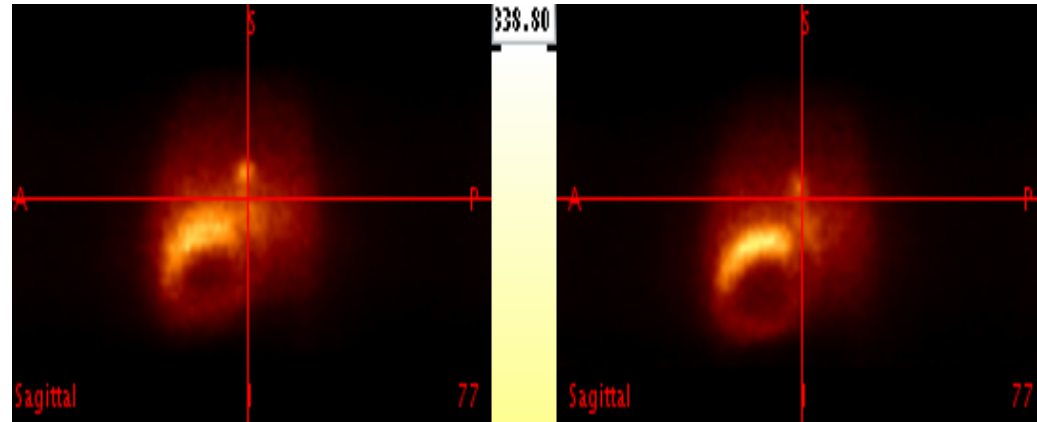
- **Voxelised Source**

  - 4D NCAT

    - Attenuation Modeling
    - Lesion
    - 80 frames / 10 cycles



128x128x55 matrix of frame with 320mm length was centered in the FOV with 180mm length along Z axis.



Summed frames 1-8

Corrected frames 1-8

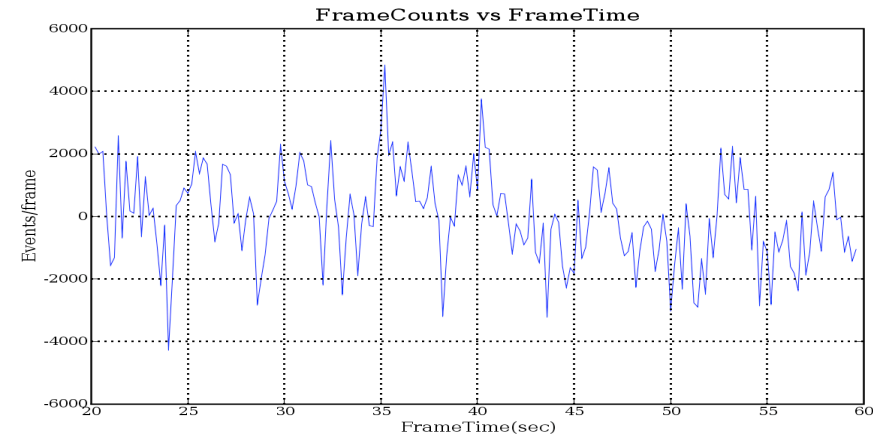
# Respiratory Motion

## Geometric Sensitivity Correction

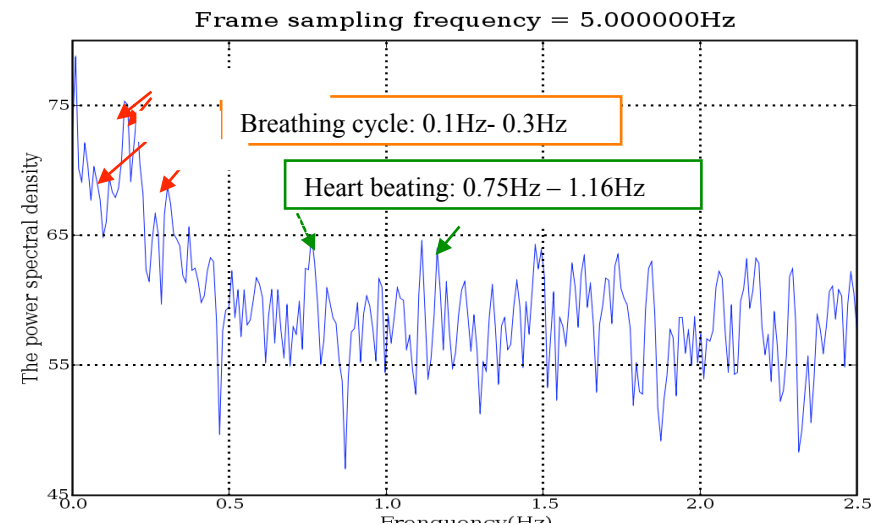
- **Clinical**

- Patient **P3969**

- NSCL cancer
- Philips Allegro PET scanner
- 381.5 MBq  $^{18}\text{F}$ -FDG
- Listmode acquisition
- coincidence rate is 226 kcps
- 57 million prompt events
- 300 seconds acquisition
- 2 million gated events.



LOR events (mean corrected) of the measured raw frames per 0.2sec from list-mode data. Baseline drift over 60 seconds is evident. The count-rate variation illustrating = the respiratory cycle.



The Power Spectral Distribution of Event Rate demonstrates several distinct frequencies; Respiratory/Cardiac features are indicated by red and green arrows respectively.

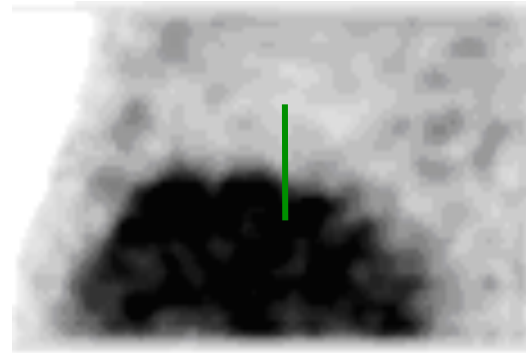
# Respiratory Motion

## Geometric Sensitivity Correction

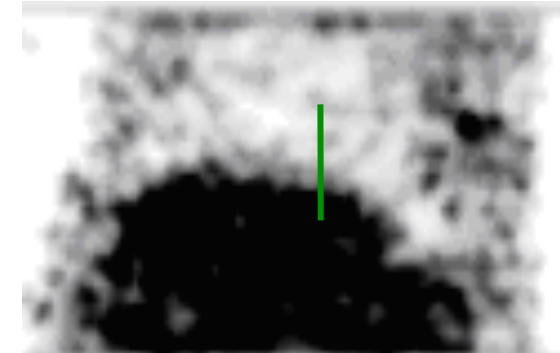
- Clinical

- Patient **P3969**

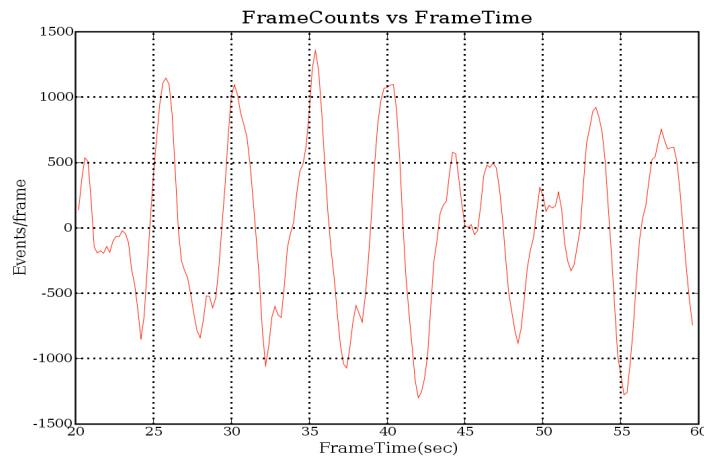
- NSCL cancer
    - Philips Allegro PET scanner
    - 381.5 MBq  $^{18}\text{F}$ -FDG
    - Listmode acquisition
    - coincidence rate is 226 kcps
    - 57 million prompt events
    - 300 seconds acquisition
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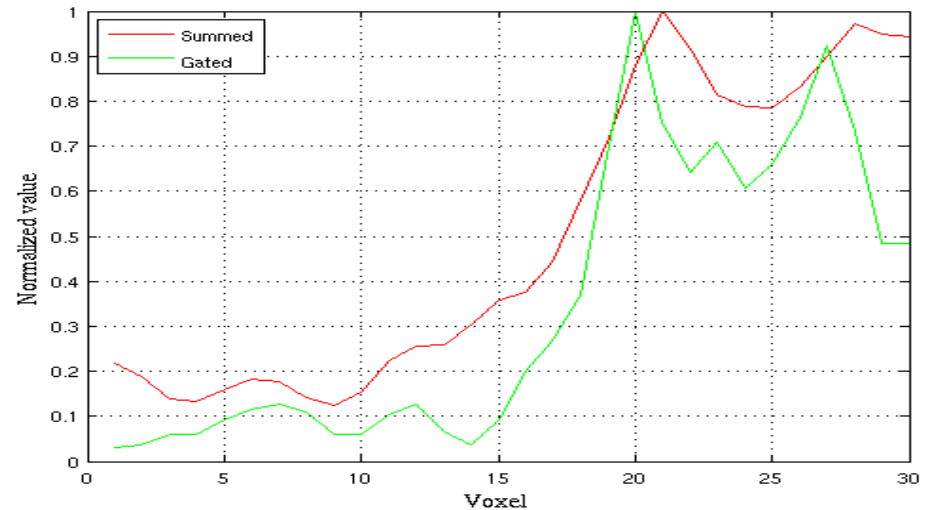
Reconstructed sum image: 1500 frames at sagittal



Reconstructed gated image: 46 frames at sagittal



Band pass filter frame events (0.1 Hz – 0.3 Hz)



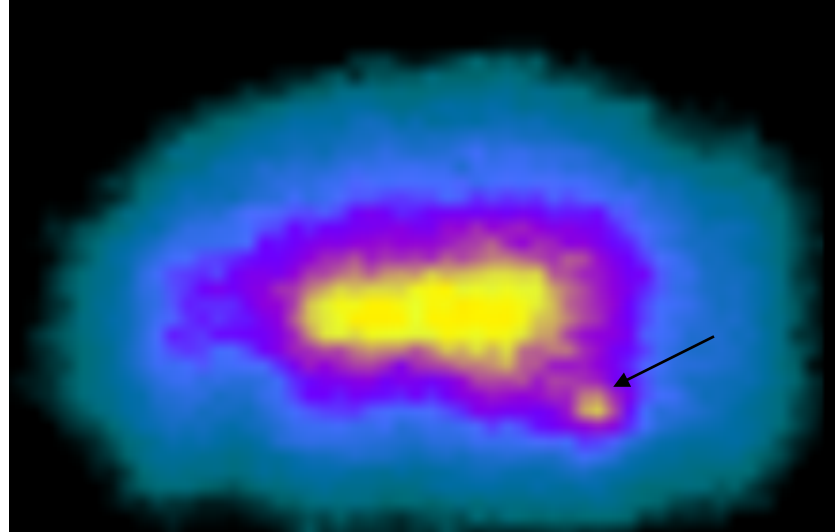
Comparison of line profile from the summed and gated reconstructed images at sagittal. The gated profile demonstrates an improved spatial contrast

# Respiratory Motion

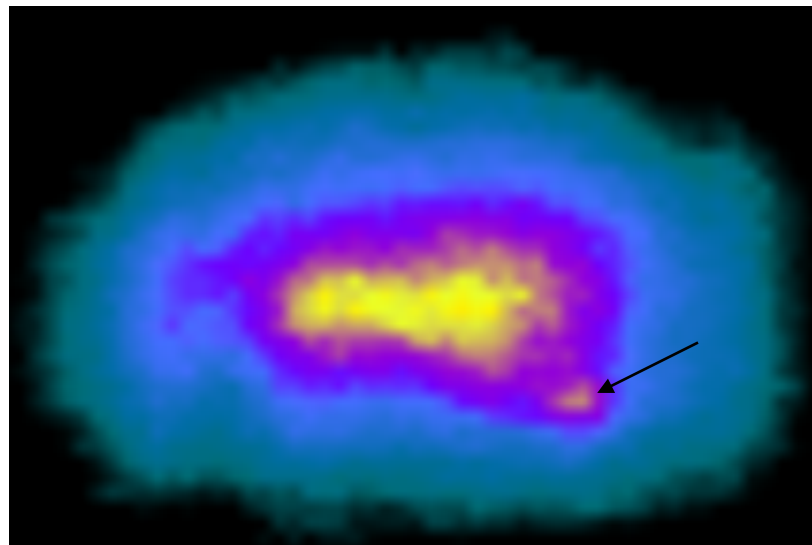
## Geometric Sensitivity Correction

- **Clinical**

- Patient **P107529**
  - NSCL Cancer
  - Philips Gemini PET scanner
  - ~370 MBq  $^{18}\text{F}$ -FDG
  - Listmode acquisition
  - 180 seconds acquisition



Summed 296 frames transaxial

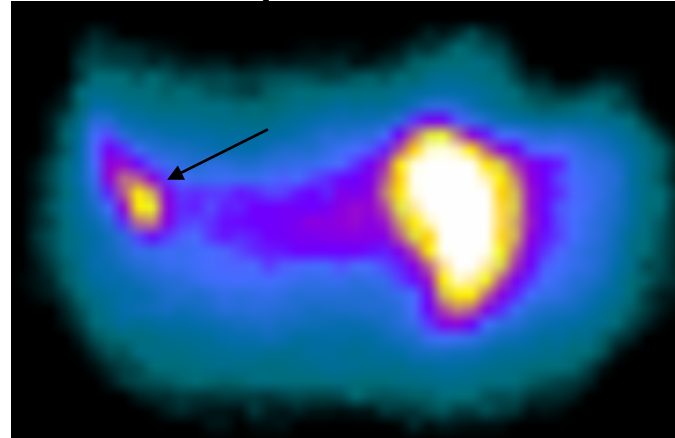


# Respiratory Motion

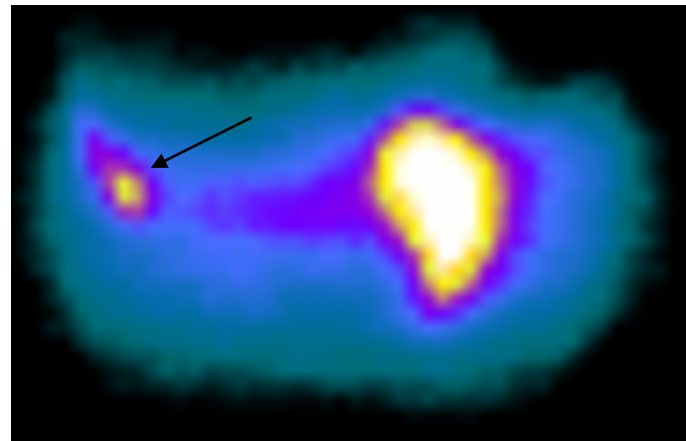
## Geometric Sensitivity Correction

- **Clinical**

- Patient **P107909**
  - NSCL Cancer
  - Philips Gemini PET scanner
  - ~370 MBq  $^{18}\text{F}$ -FDG
  - Listmode acquisition
  - 180 seconds acquisition



Summed 360 frames at coronal



Corrected 360 frames, 0.5s per frame, 12mm amplitude at coronal

8th December, 2008



Austin Health

# Summary

1

## Simulation

### GATE & NCAT Evaluation

- Geometric Phantom
- Voxelized Phantom

### GSG & GSC Validation

#### ◆ GSG

- Geometric Phantom
- Voxelized Phantom

#### ◆ GSC

- Geometric Phantom
- Voxelized Phantom

2

## Clinical

#### ◆ GSG

- One clinical data with non tumor

#### ◆ GSC

- Two clinical data with tumor



# Conclusion

Respiratory motion gating and correction

Utilising the geometric sensitivity properties of 3D PET.

Data-driven method is intrinsic to acquired list-mode.

Does not involve hardware monitoring.

All simulations and clinical studies demonstrate that the proposed GSG & GSC method is able to compensate respiratory motion.



# Acknowledgements

- Department Nuclear Medicine & Centre for PET, Austin Health
  - Dr Jianfeng He
  - Dr. Sylvia J. Gong
  - Tim Saunder
  - Gareth Jones
  - Prof. Andrew M. Scott
  
- School of Medical Sciences, RMIT
  - A/Prof. Moshi Geso
  - Trevor Ackerly
  
- Philips Research Division, Aachen, Germany
  - Dr. Ralph Brinks

