

SPECT: Current Status, Future Directions

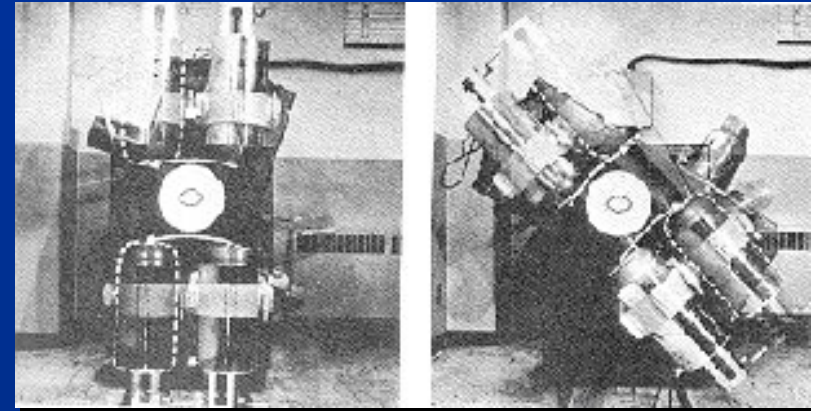
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University of Wollongong.*

Outline

- instrumentation
- reconstruction
- quantitative corrections
- opportunities for development



SPECT: historical background



1959 - The world's first transverse section emission tomographic image was obtained by David Kuhl and Roy Edwards

1963 - Kuhl and Edwards developed an emission tomography system which became the precursor to SPECT

1973 - publication on Aberdeen section scanner

1976 - first gamma camera SPECT system introduced by Keyes

1983 - commercial gamma camera SPECT introduced

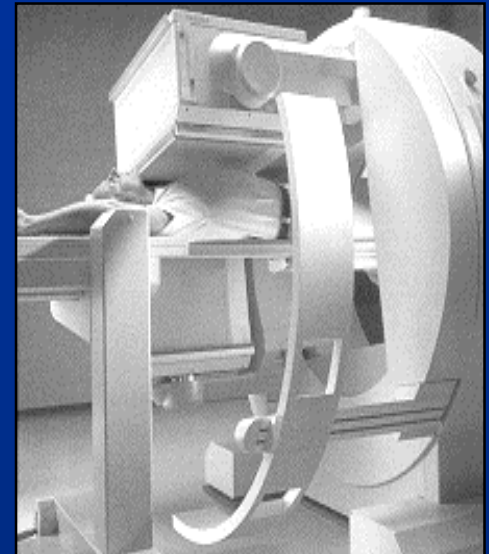
.....

2003 - attenuation corrected SPECT using iterative reconstruction

SPECT:

current standard practice (basic!)

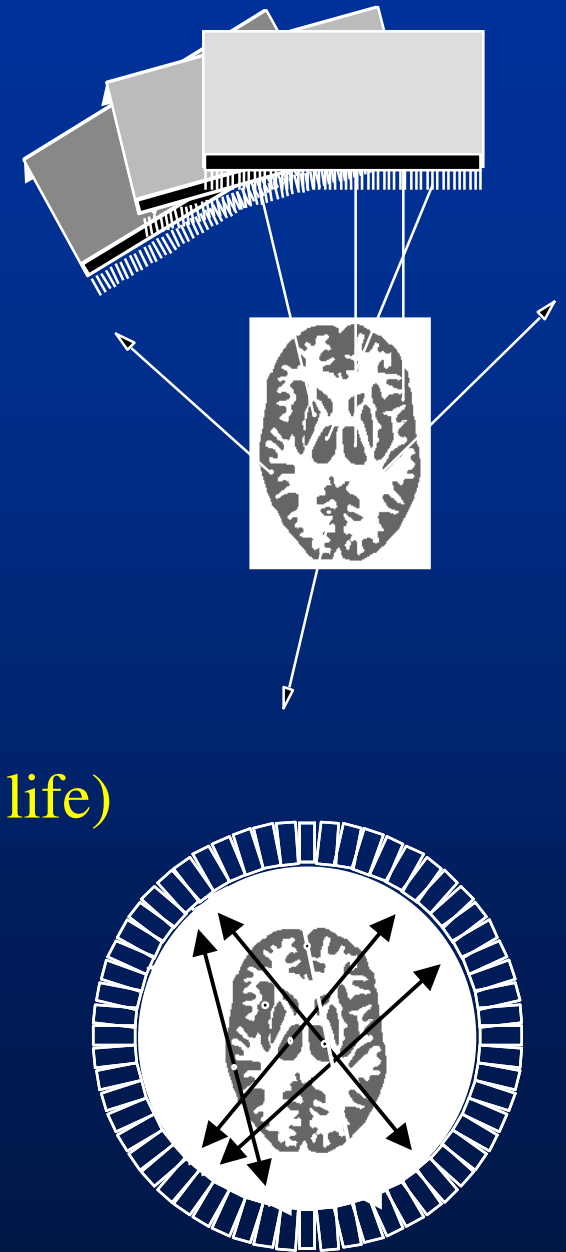
- dual head acquisition
- filtered back projection
- gated cardiac acquisition
- dynamic acquisition (never)
- Chang attenuation correction (sometimes)
- measured transmission (available at few sites)
- iterative reconstruction (available but underutilised)
- scatter correction (limited use)
- motion correction (available but crude!)
- resolution compensation (not usually available)
- partial volume correction (what's this?)



SPECT: how different is it from PET?

- similar resolution possible
- lower attenuation
- less attenuation correction artefacts
- less scatter (compared to 3D PET)
- lower radiation dose
- more convenient radionuclides (longer half life)
- less expensive
- similar reconstruction methods
- **LOWER SENSITIVITY**
- **more noise, longer acquisition... etc.**

see: Bailey, Eur J nucl Med, 2003; 30: 1046-1049.



Instrumentation

old ideas being brought to reality

High resolution small animal systems

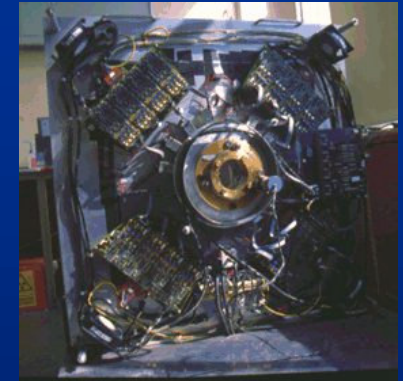
- dedicated systems with small detectors
- pinhole tomography
- coded aperture imaging

Application specific systems

- dedicated breast imaging
- high resolution brain SPECT

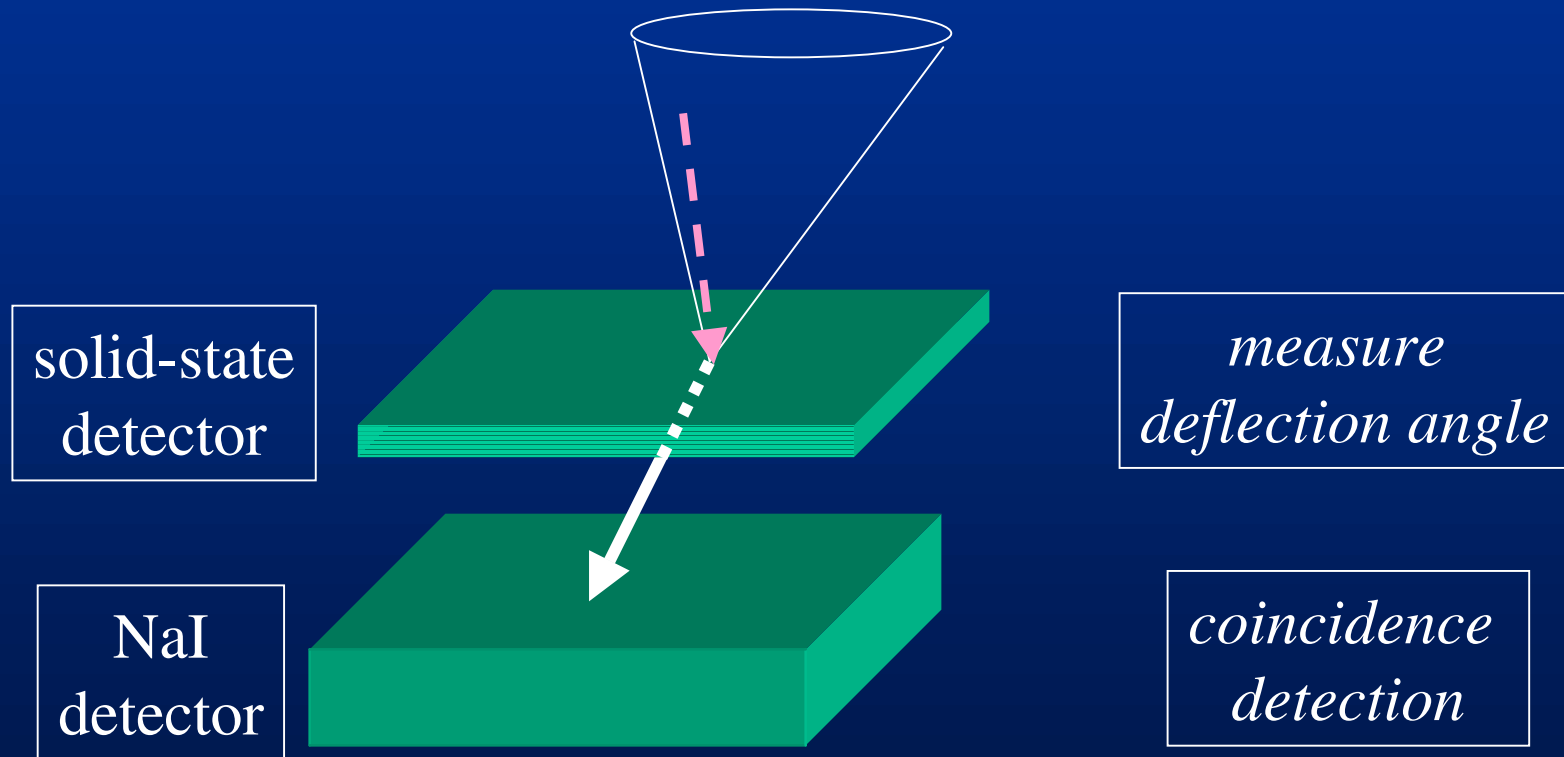
High sensitivity systems

- rotating slat collimator
- Compton camera



Instrumentation: Compton camera

replaces collimator with solid state detector (high energy resn)



potential sensitivity gain of 20 (Univ of Michigan)

Instrumentation:

Limitations in what the suppliers provide

- transmission measurement (reliability)
- dynamic SPECT (some capability)
- multiple energy windows (supplier dependent)
- dynamic projections
- listmode acquisition
- respiratory gating
- alternative collimators (e.g. pinhole)
- hybrid systems (i.e. CT)
- variation in implementation
- lack of verification tools
- concern regarding cross-comparison



Reconstruction

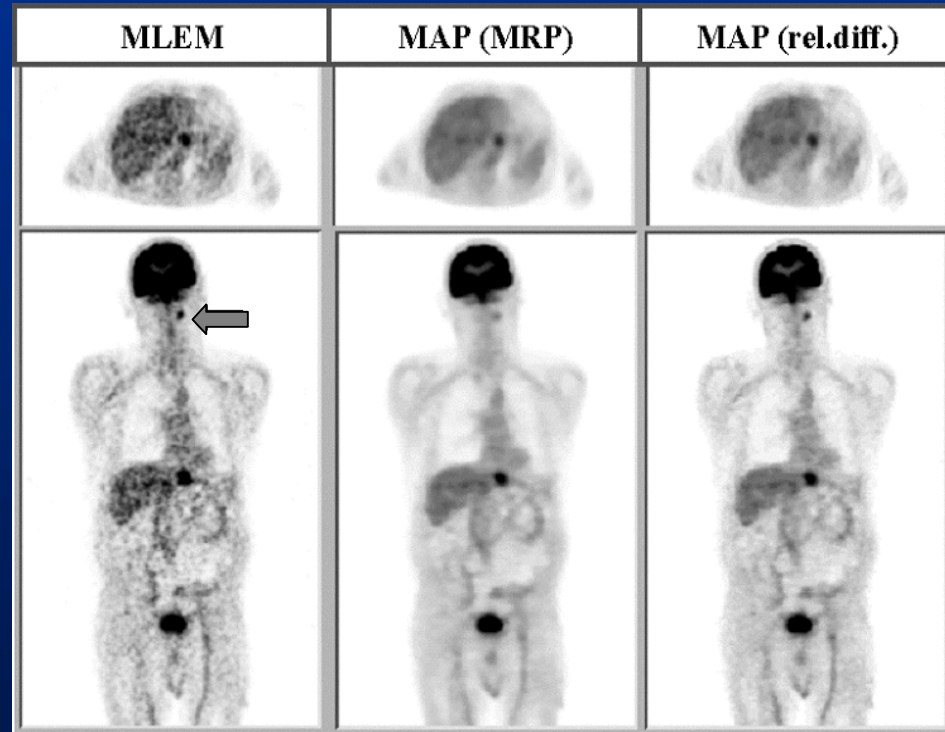
Poor understanding of when to use iterative methods

what is effect?

- contrast
- noise appearance
- lesion detectability
- quantitative accuracy

new initiatives

- novel geometry
- approaches to noise
- 3D and 4D models
- Monte Carlo

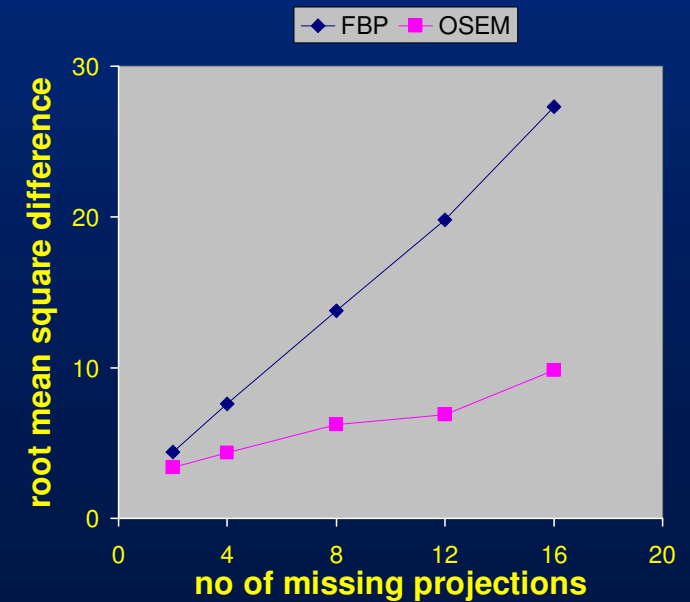
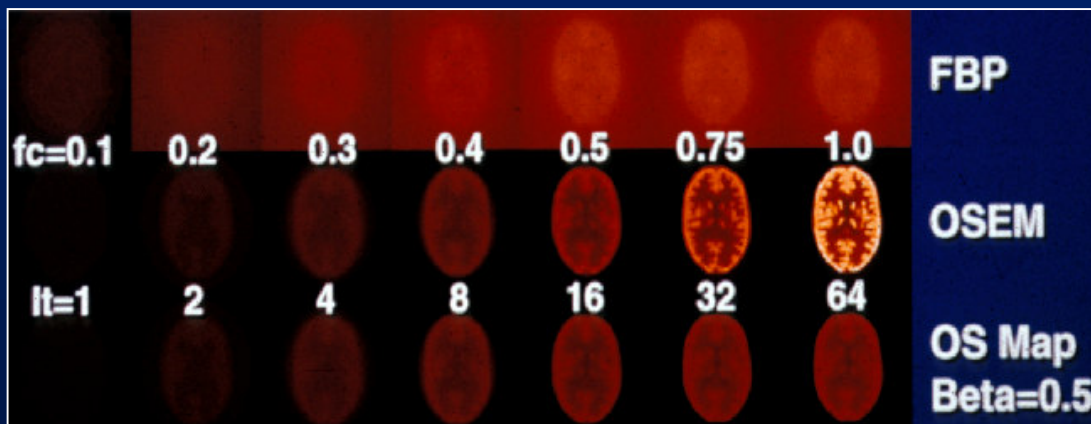
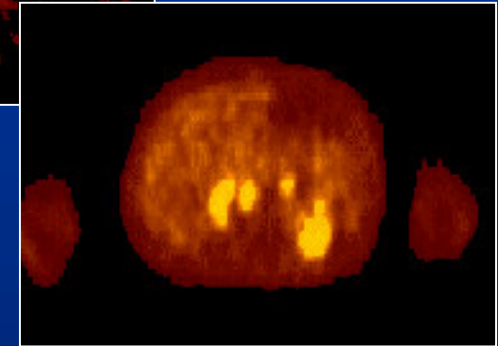
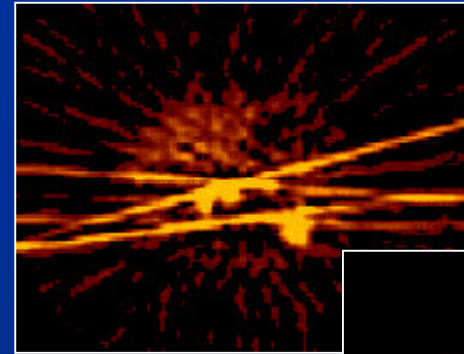


Hutton, Nuyts, Zaidi: 2003

Reconstruction: OSEM

Available, fast and useful

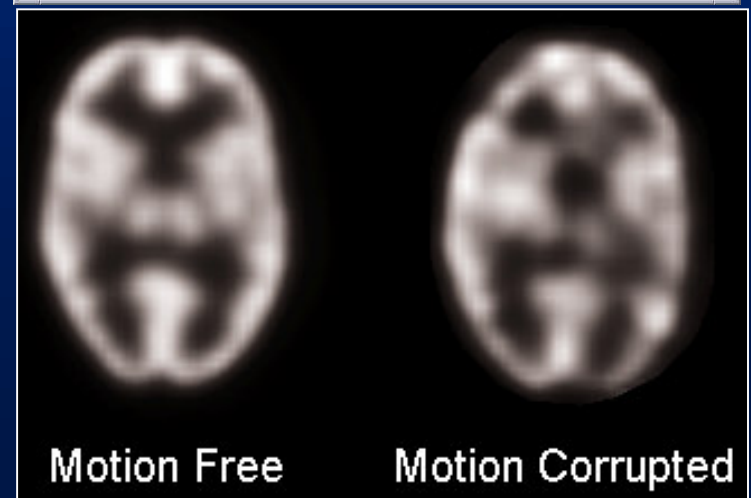
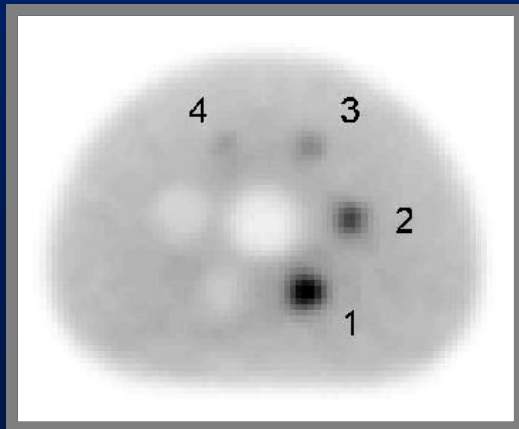
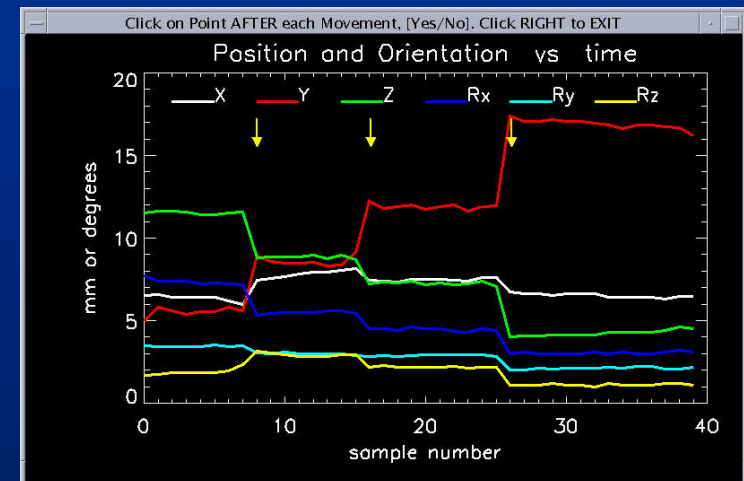
- attenuation correction
- noise reduction (background)
- streak removal
- handles missing data
- flexible (attenuation, motion etc)



Corrections

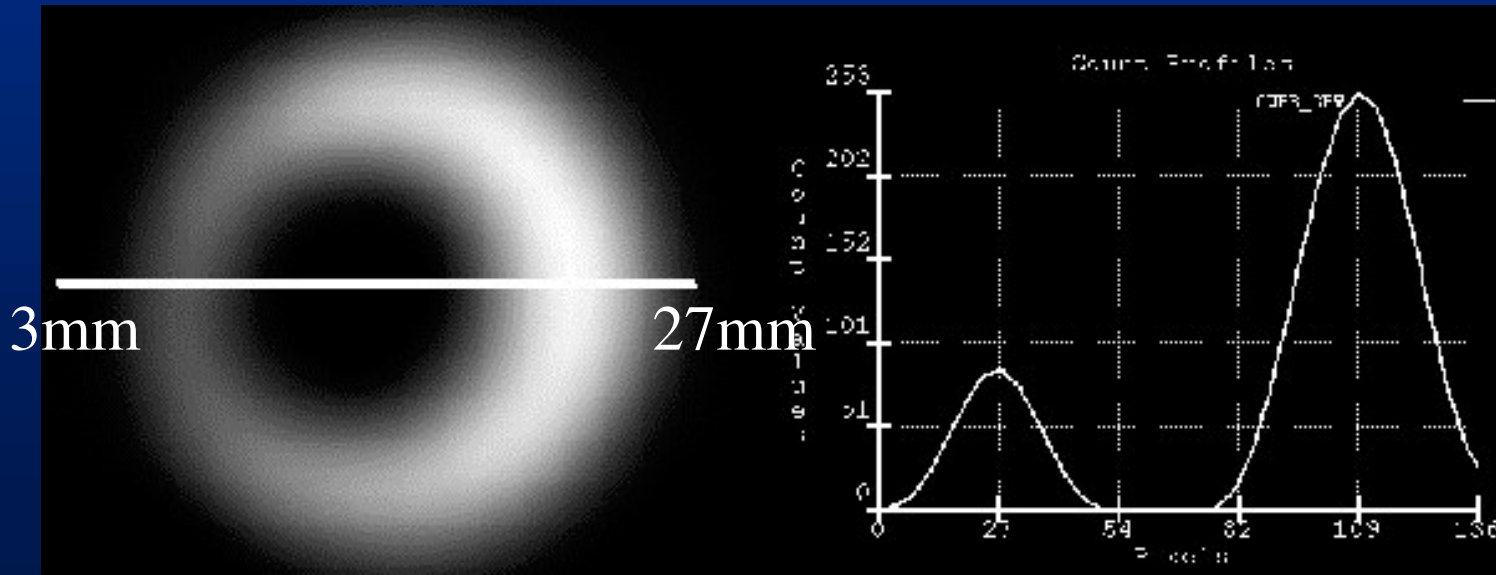
Need better understanding of importance

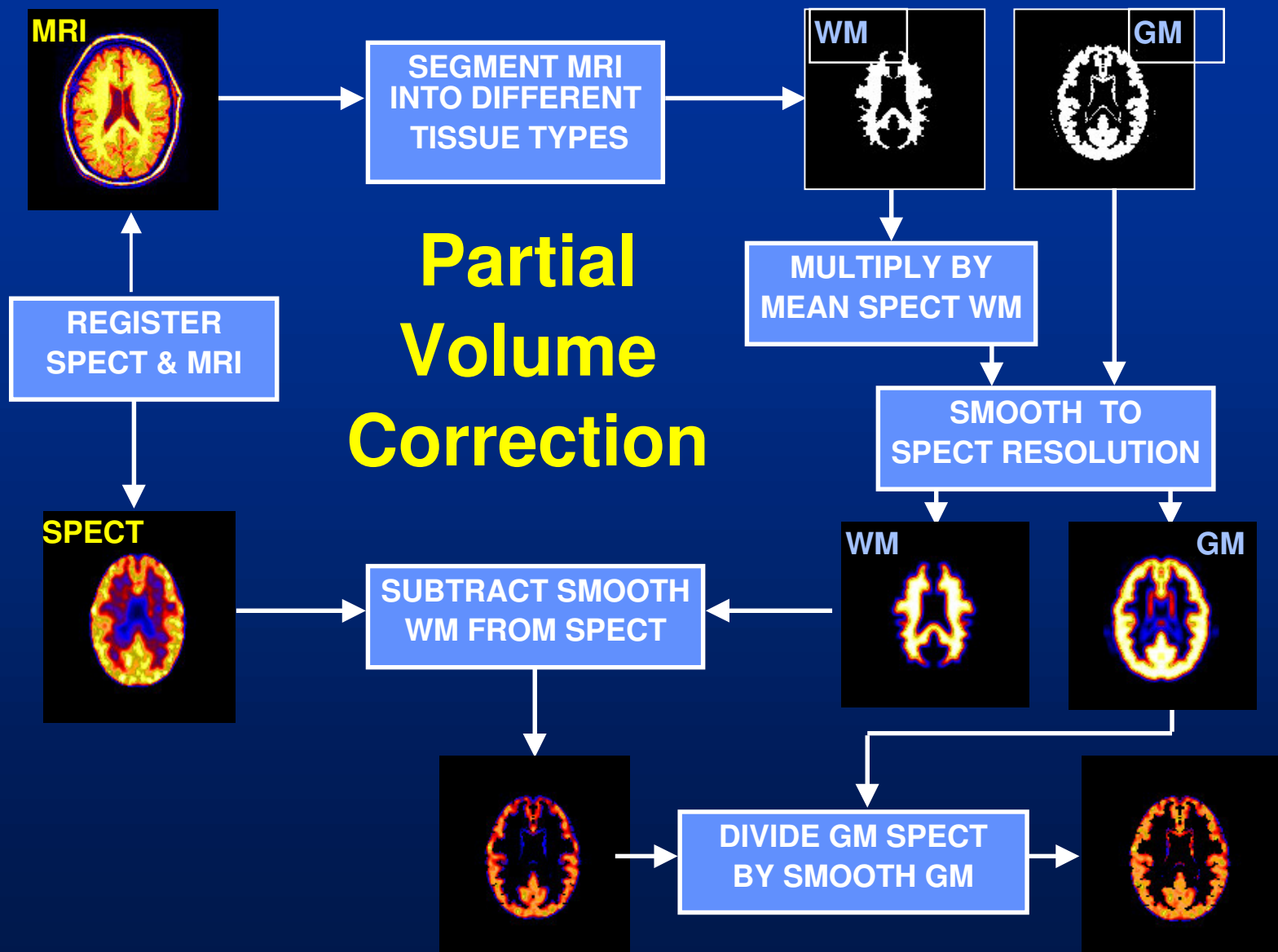
- attenuation correction
- scatter correction
- resolution compensation
- partial volume correction
- motion correction



'Partial volume' effect

- difficult to identify
- usually not possible to distinguish count reduction from change in wall thickness

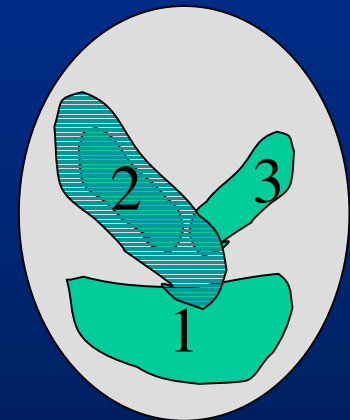




Region-based ‘geometric transfer matrix’

(Rousset 1998)

- segment anatomical regions for structures or tissues
- smooth regions to match emission resolution
- define contribution of activities in structures to each region (geometric transfer matrix: w_{ij})
- solve for activity in each region (T_i), given measurement (t_j)



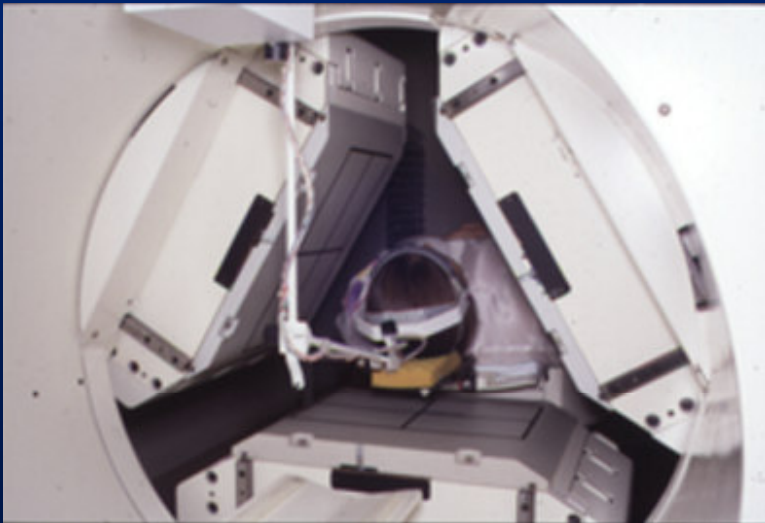
$$t_j = \sum_i w_{ij} T_i$$

	w_{ij}	structure (i)	
region (j)	0.8	0.1	0.1
	0.05	0.65	0.1
	0.05	0.1	0.65

diagonal: RC; other: spillover

Motion measurement

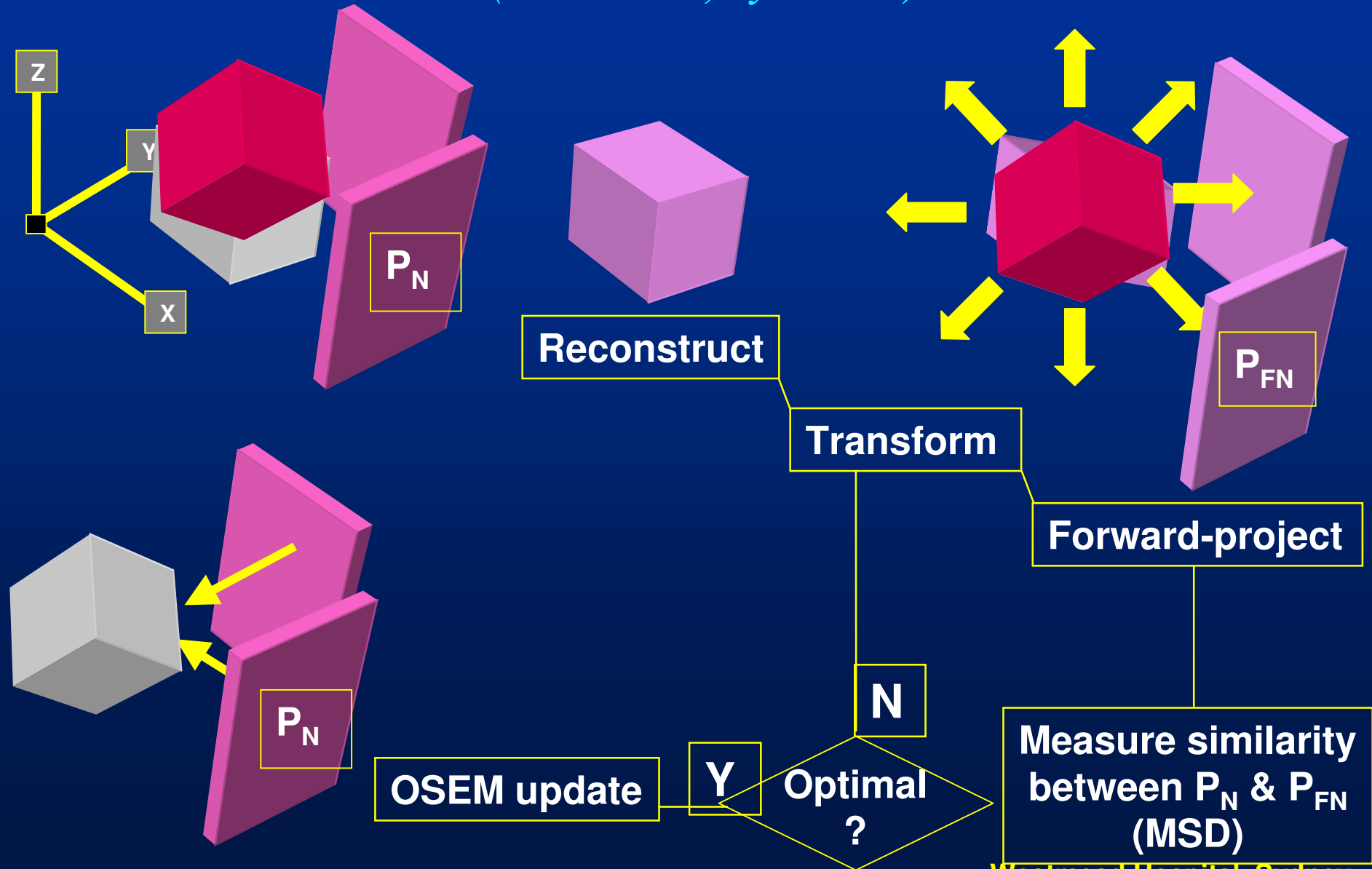
- external markers
- video camera
- electro-mechanical device
- electro-magnetic device
- opto-electronic device (polaris)
- data-driven



Westmead Hospital, Sydney

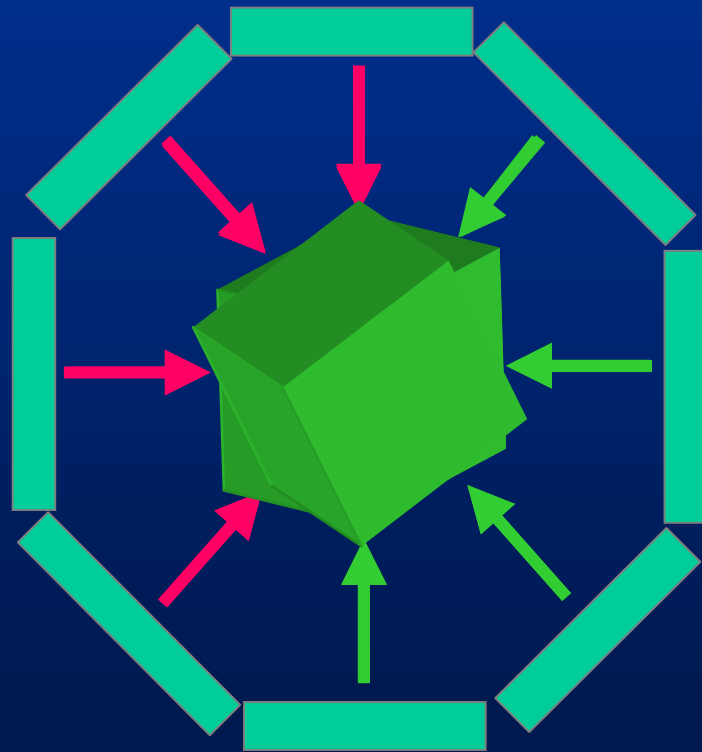
Data-Driven Motion Correction

(Hutton 2002, Kyme 2003)



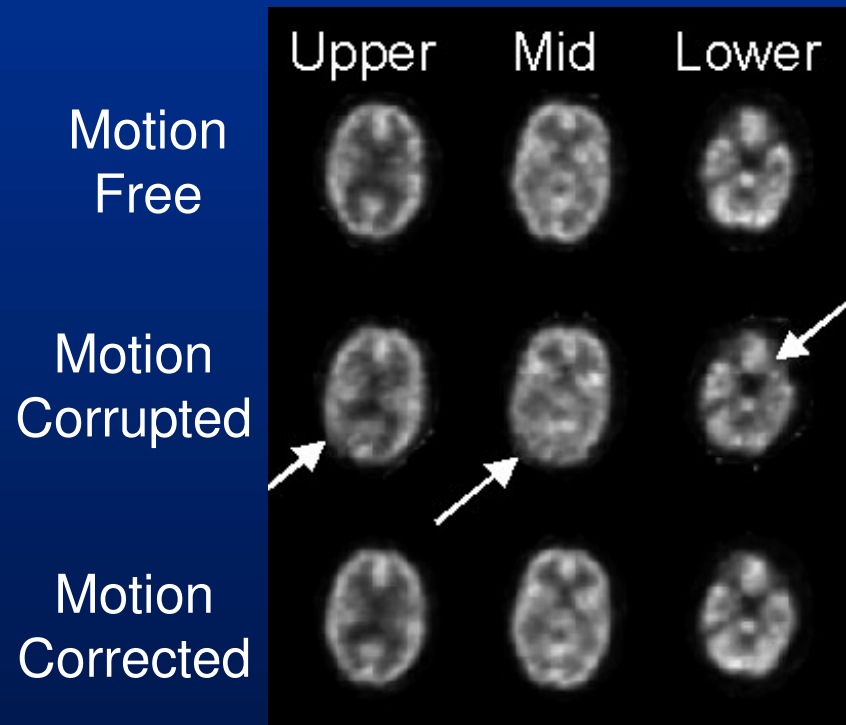
OSEM reconstruction given measured or estimated motion

Use Compton reconstruction



 Subset 1

 Subset 2

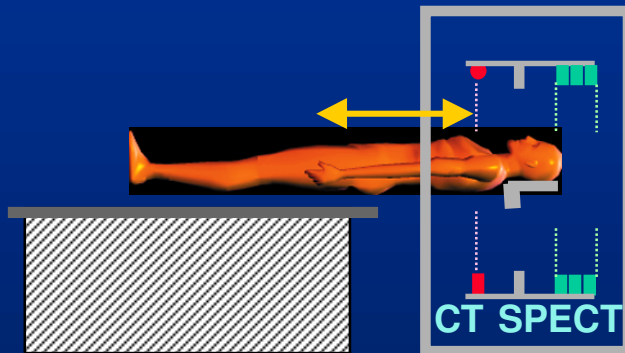


three discrete positions

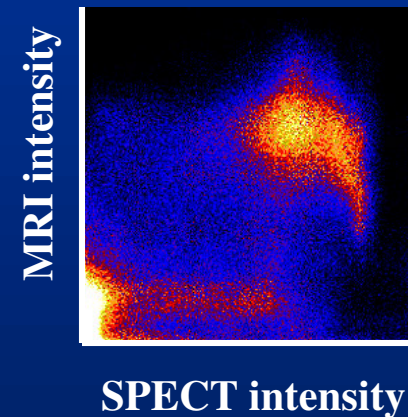
Opportunities for development

Multi-modality imaging as a precursor for advanced analysis

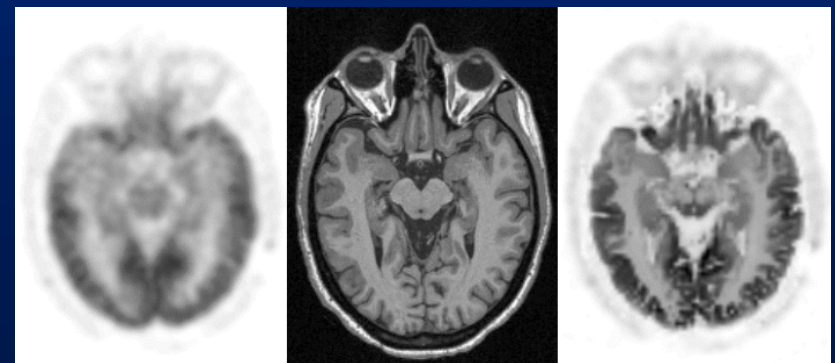
hardware



software

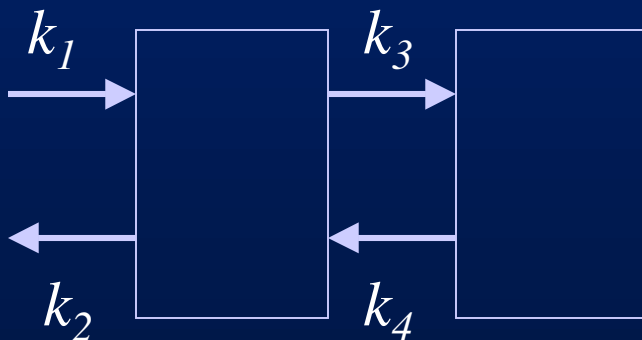
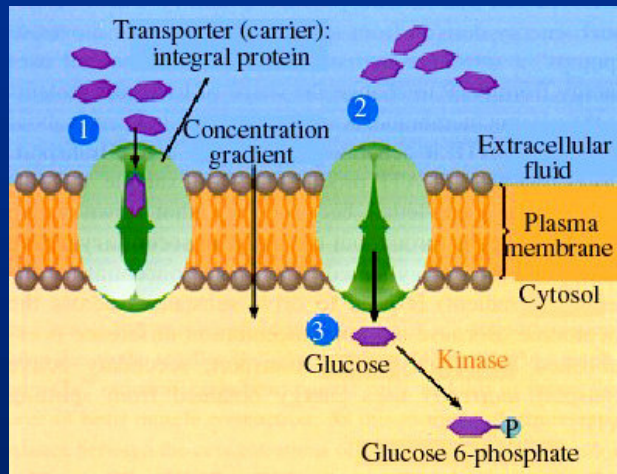


- functional parameter fusion
- partial volume correction
- motion correction
- segmentation and shape analysis
- resolution enhancement



Opportunities for development

Quantification of functional parameters: single photon tracers



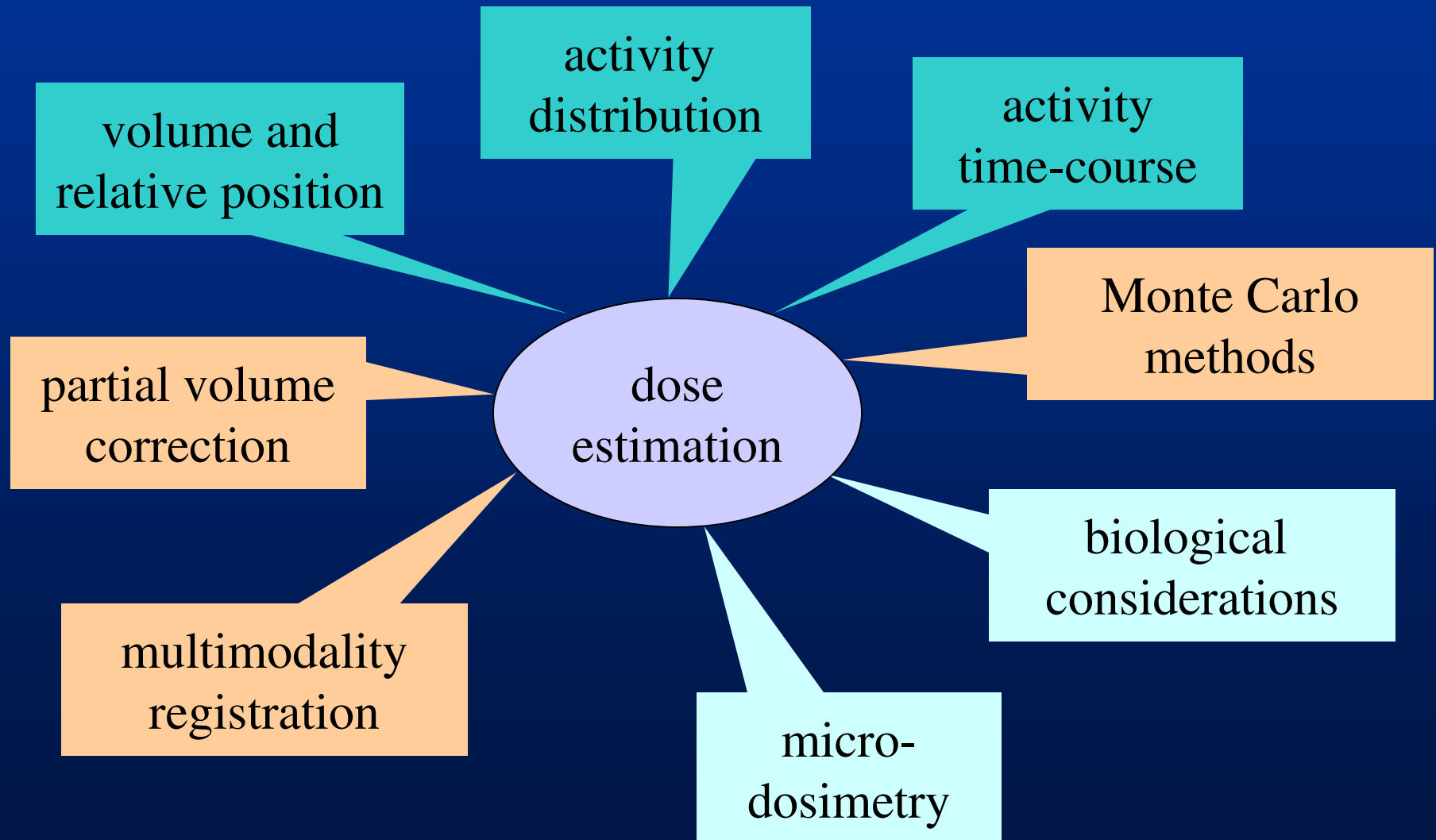
Tracer kinetic models

- simplified ROI parameters
- graphical analysis (e.g. Patlak)
- study decomposition
- compartmental models
- mixture models
- spectral analysis
- dynamic models
- interventional models
- microscopic models

Opportunities for development



Patient specific dosimetry using unsealed sources



SPECT

Current status: the backbone of Nuclear Medicine

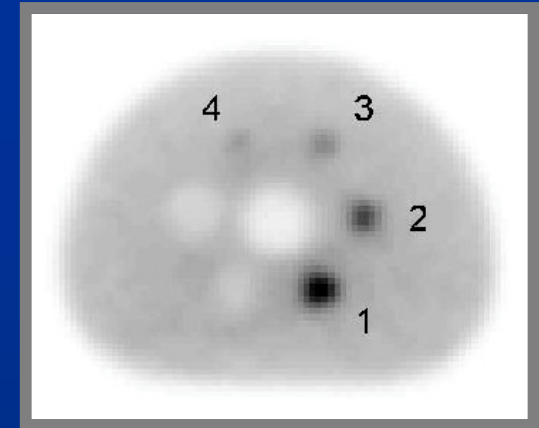
Future directions: quantitative molecular studies

A program of relevant topics

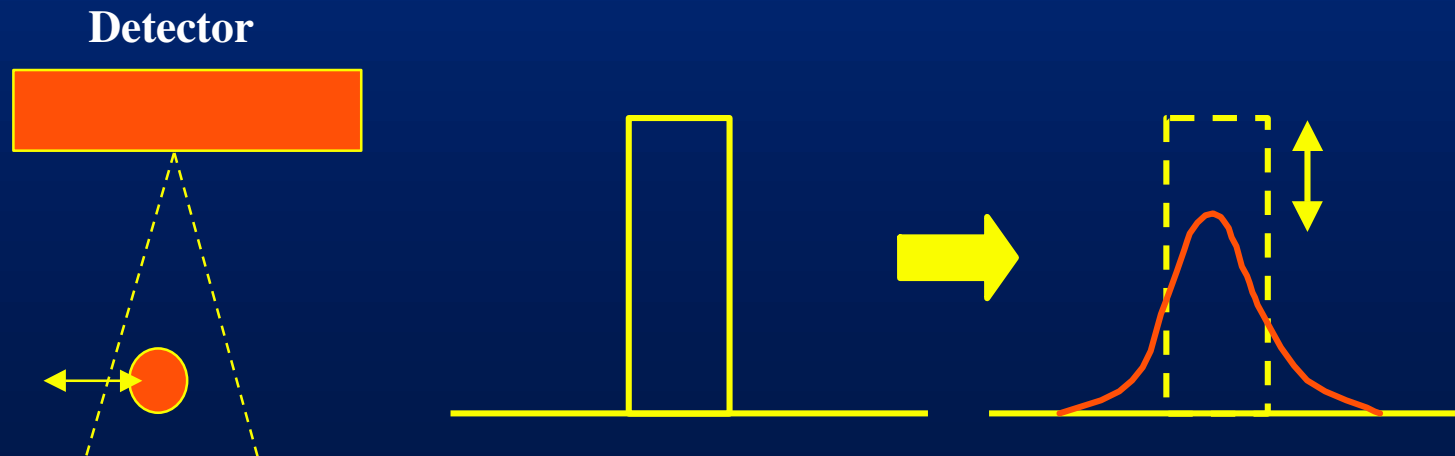
- dynamics and tracer kinetics
- transmission scanning
- industry developments
- new tracers
- small animal systems
- radionuclide therapy planning
- clinical perspective



'Partial volume' effect (*limited resolution effect*)



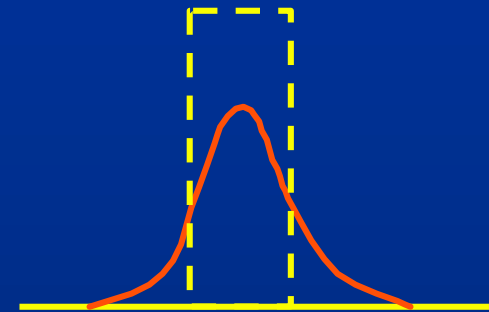
When an object partially occupies the sensitive volume of an imaging instrument (in space or time) the measured signal is reduced in amplitude.



Activity concentration: counts / volume

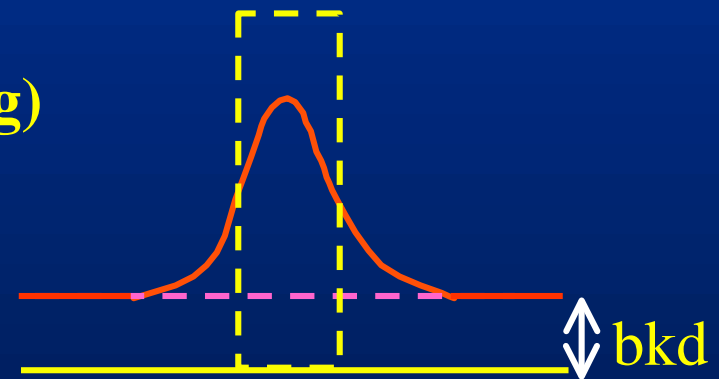
- no background or adjacent activity

$$\frac{\text{total counts}}{\text{actual volume}}$$



- background (e.g. non-specific binding)

$$\frac{\text{total counts} - \text{bkd}}{\text{actual volume}}$$



- spillover correction (adjacent activity)

$$\frac{\text{total counts} - \text{estimated bkd}}{\text{actual volume}}$$

